

First Insights on the Upcoming Role of Next-Generation PLLA-LASYNPRO™ in Aesthetic and Regenerative Medicine. A Survey of Experts—Foundations and Rationale

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Article

First Insights on the Upcoming Role of Next-Generation PLLA-LASYNPRO™ in Aesthetic and Regenerative Medicine. A Survey of Experts—Foundations and Rationale

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Abstract: How injectable collagen stimulators promote the neosynthesis of collagen and other components of the extracellular matrix in connective tissues has typically been linked to an inflammatory foreign-body reaction (FBR). A shift from the long-dominant inflammatory FBR paradigm to a new focus on non-inflammatory collagen and extracellular matrix regeneration may have emerged with the next-generation PLLA-LASYNPRO™ microspheres of the CE-approved JULÄINE™ medical device, which preclinical studies suggest are negligibly likely to trigger inflammation. A survey and subsequent discussions during a board meeting held in Milan, Italy, which involved thirteen distinguished experts in micro-invasive aesthetic medicine, aesthetic plastic surgery, and dermatology, led to this document and the accompanying manuscript “First Insights on the Upcoming Role of Next-Generation PLLA-LASYNPRO™ in Aesthetic and Regenerative Medicine. A Survey of Experts — Practical Suggestions”. This first paper outlines the initial insights and discussion of the experts on the basis and the value of the non-inflammatory rationale proposed for PLLA-LASYNPRO™ subdermal implants in aesthetic and regenerative medicine.

Keywords: earlier-generation poly-L-lactic acid; extracellular matrix regeneration; foreign body response; injectable collagen stimulators; expert board; PLLA-LASYNPRO™, skin quality

Neosynthesis of Collagen and Extracellular Matrix: The Long-Dominant Foreign Body Reaction Paradigm

Since the introduction of the first sterile, water-reconstituted poly-L-lactic acid (PLLA) formulation around the turn of the century, the notion of an inflammatory foreign-body reaction (FBR), whether acknowledged or downplayed, has been central to understanding how injectable resorbable collagen stimulators enhance the synthesis of collagen and other components of the extracellular matrix in connective tissues [1,2]. The FBR is a spontaneous response that gradually encases and sequesters subdermal implants, such as traditional injectable collagen stimulators, in a fibrous shell. Unfortunately, inflammation also contributes to the most severe late side effects, including nodules and hardened skin indurations, which can occasionally progress into persistent granulomas lasting for months or even years (Figure 1) [1].

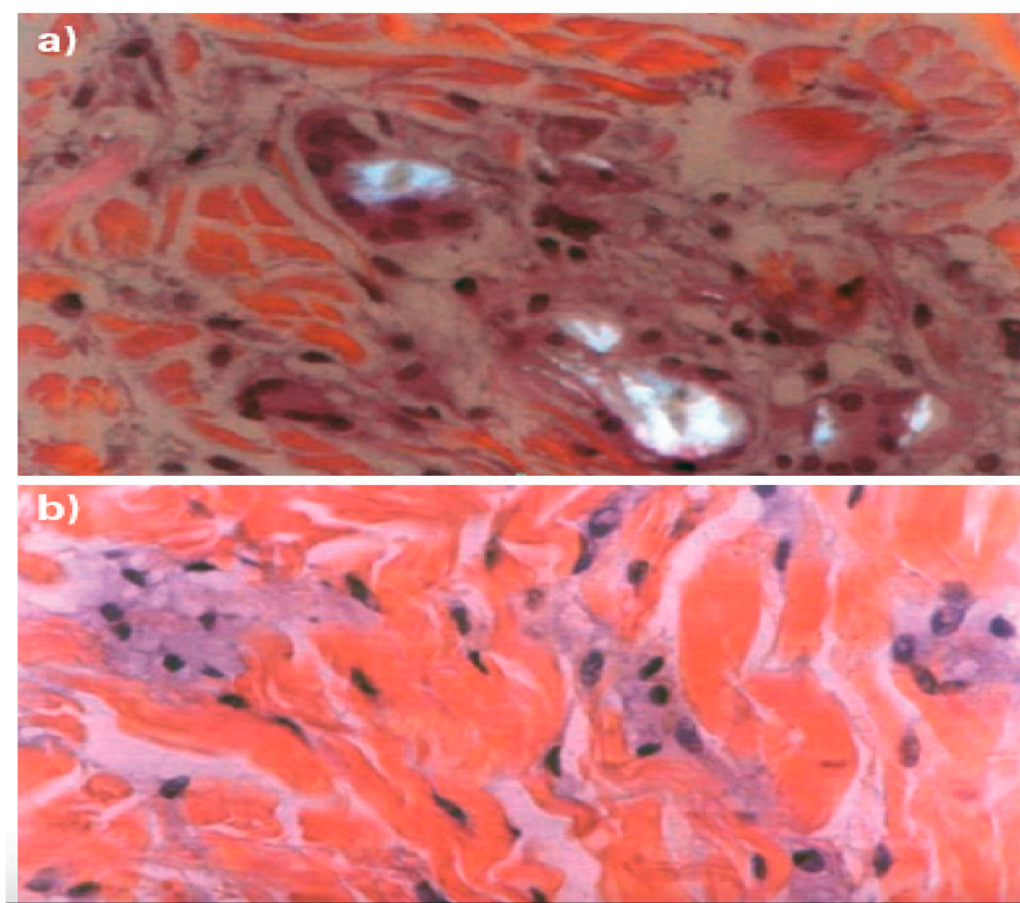


Figure 1. (a) Ongoing inflammatory foreign-body response, characterized by inflammatory giant cells and histiocytes, observed twelve months after the injection of sterile water-reconstituted PLLA microparticles. The PLLA microparticles appear to be waning, and there is widespread evidence of neocollagenesis. (b) No residual PLLA microparticles, but persisting inflammatory infiltrates thirty months after injection. Hematoxylin and eosin staining, X400 magnification. Credit for the reprinted image with sought permission: Ref. [1].

A 2021 multicenter, retrospective chart review of U.S. medical records involving 4,483 treatments across the midface, temple, and jawline in 1,002 subjects revealed a persistently concerning long-term incidence of nodules at 0.4% for early-generation PLLA despite reconstituting the dry powder to 8-10 mL [3]. Other recent reviews indicate that the long-term incidence of late adverse effects—including nonvisible but palpable subcutaneous nodules, visible nodules, and chronic granuloma—ranges from a non-negligible 0.2% to 1.2% [4]. The burden of inflammatory late adverse effects appears unrelated to geographical latitude and ethnicity. Moreover, it is likely underestimated due to diagnostic challenges and the late occurrence, which masks the cause-and-effect relationship [5].

Inflammatory side effects do not exempt the injectable collagen bio-stimulator poly(ϵ -caprolactone) or PCL; however, they occur only occasionally and are significantly milder, as

confirmed by the U.S. FDA Center for Devices and Radiological Health (Figure 2) [2,6]. According to a 2020 review of PCL, *"The host response includes protein coating of the material, macrophage migration, and encapsulation at around three weeks. Inflammatory reactions and wound healing pathways participate in this stepwise repair process"* [7].

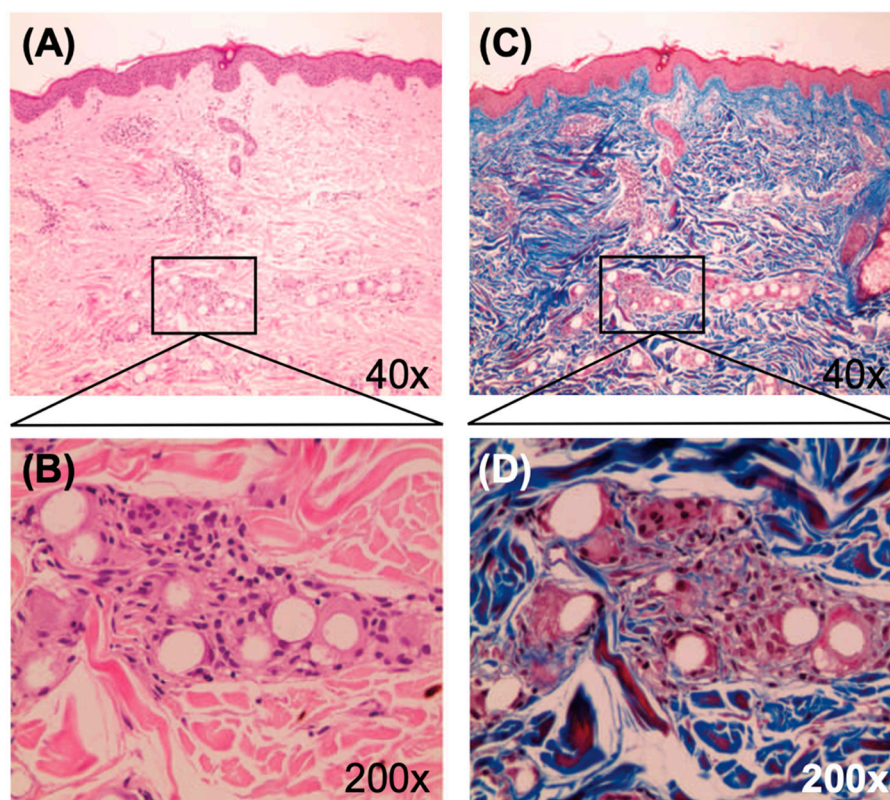


Figure 2. Dense collagen fibers and a mild fibroblastic and histiocytic foreign body-like response surround poly(ϵ -caprolactone) microspheres thirteen months after poly(ϵ -caprolactone) treatment. Staining: hematoxylin-eosin (A and B) and Martin's trichrome (C and D); magnification: X40 (A and C) and X200 (B and D). Credit for the reprinted image with sought permission: Ref. [2].

Invoking the inflammatory FBR postulate seems less convincing for resorbable ceramic-derivative calcium hydroxylapatite. Unlike conventional PLLA microparticles, the macrophage expression of several pro-inflammatory cytokines, including IL-1 α , IL-1 β , IL-8 β , and Chemokine (C-X-C motif) Ligand 6 (CXCL6), appears significantly downregulated after exposure to the calcium hydroxylapatite microspheres [8,9]. However, other evidence seems to contradict these findings. Inflammatory biomarkers such as Chemokine (C-X-C motif) Ligand 8/IL-8 (CXCL8/IL-8), IL-6, and prostaglandin-endoperoxide synthase 2 (PTGS2) increase with calcium hydroxylapatite implants in over half of a panel of subjects treated for nasolabial folds [10]. Furthermore, compared with conventional PLLA in the opposing arms of the five female subjects following superficial subcutaneous injection, histology revealed a similar new production of collagen and elastic fibers and a comparable moderate to intense inflammatory reaction involving lymphocytic and giant cell infiltrate [11]. More generally, the most recent literature does not exclude the evidence of focal accumulations and nodules with calcium hydroxylapatite [12].

Is It Conceivable to Progress Beyond the Foreign Body Response in Skin Connective tissue Regeneration?

The FBR postulate has never been denied or refused, although international literature has occasionally downplayed the inflammatory nature of induced extracellular matrix regeneration. A

shift from the inflammatory FBR paradigm to a novel non-inflammatory collagen/ECM regeneration that mitigates the risks of delayed inflammatory side effects and improves skin physiology may have emerged with the next-generation PLLA-LASYNPRO™ microspheres. These highly uniform microspheres, produced using advanced patented freeze-drying technologies, are negligibly prone to disrupting phagosome membranes and causing the pro-inflammatory leakage of cathepsin into the cytosol. Furthermore, the new-technology, smooth-surfaced, rounded poly-L-lactic acid microparticles preferentially activate the subpopulation of M2-polarized macrophages that secrete anti-inflammatory cytokines such as interleukin-4 (IL-4), IL-10, and IL-13 [13,14].

Two decades after injectable poly-L-lactic acid received approval in Europe (1999) and the United States (2004) [15], the PLLA-LASYNPRO™ subdermal implants and the JULÄINE™ medical device aim to signify a significant turnaround. 2are currently underway in Europe to validate the non-inflammatory rationale behind the new-technology PLLA ingredient and its anticipated efficacy and safety benefits through methodologically sound, high-quality studies. A recent Spanish interim multicenter analysis on 36 adult subjects confirmed the safety and rejuvenating efficacy of the PLLA-LASYNPRO™ microsphere implants on mild to severe nasolabial folds [16]. Assessed with two photo-numeric tools, the five-grade WSRS (Wrinkle Severity Rating Scale) and the six-point MFVDS (Midface Volume Deficit Scale focused on middle third facial volume loss), 44.4% and 63.9% of subjects reported highly significant reductions, uniform on the right and left facial sides, of at least one point compared to baseline one and two months after the first injection. Procollagen type I Carboxy-terminal Propeptide (P1CP) circulating levels, a marker of type-1 collagen neosynthesis, rapidly showed significant increases one month after the first dose. Adverse effects, such as occasional edema, erythema, and infrequent local irritation, were mild, transient, and expected, typical with all micro-invasive procedures [16].

A board of thirteen experts in aesthetic and regenerative medicine, dermatology, and aesthetic plastic surgery convened to discuss and share their insights with their European colleagues about the rationale and role of PLLA-LASYNPRO™ subdermal implants drawing from the available evidence and their direct clinical experience in the clinical research program [17]. While research is progressing, the board experts believe that the results of their collaborative efforts deserve a broader audience, including a set of preliminary suggestions for integrating the novel CE-approved JULÄINE™ medical device based on PLLA-LASYNPRO™ subdermal implants into everyday regenerative medicine practice [17].

The PLLA-LASYNPRO™ Rationale Beyond the FBR Paradigm

On average, early-generation PLLA microparticles appear oblong, irregular, and heterogeneous in size and shape. They resemble irregular, spiky micro-flakes ranging from 2 to 150 µm along their longer axis, with nearly half of the microparticles measuring less than 20 µm in diameter (Figures 3A and 3B) [18–20]. This characteristic makes early-generation PLLA microparticles susceptible to an inflammatory response and phagocytosis by macrophages, which can ultimately lead to the development of granulomas and delayed-onset nodules. Additionally, the microparticles in some formulations of early-generation PLLA are porous, further influencing inflammatory responses [18–20]. Furthermore, a sizable fraction of earlier PLLA microparticles that are at least 100 µm risks becoming trapped in the standard 26-gauge needle (internal diameter: 100 µm) used for injection [18].

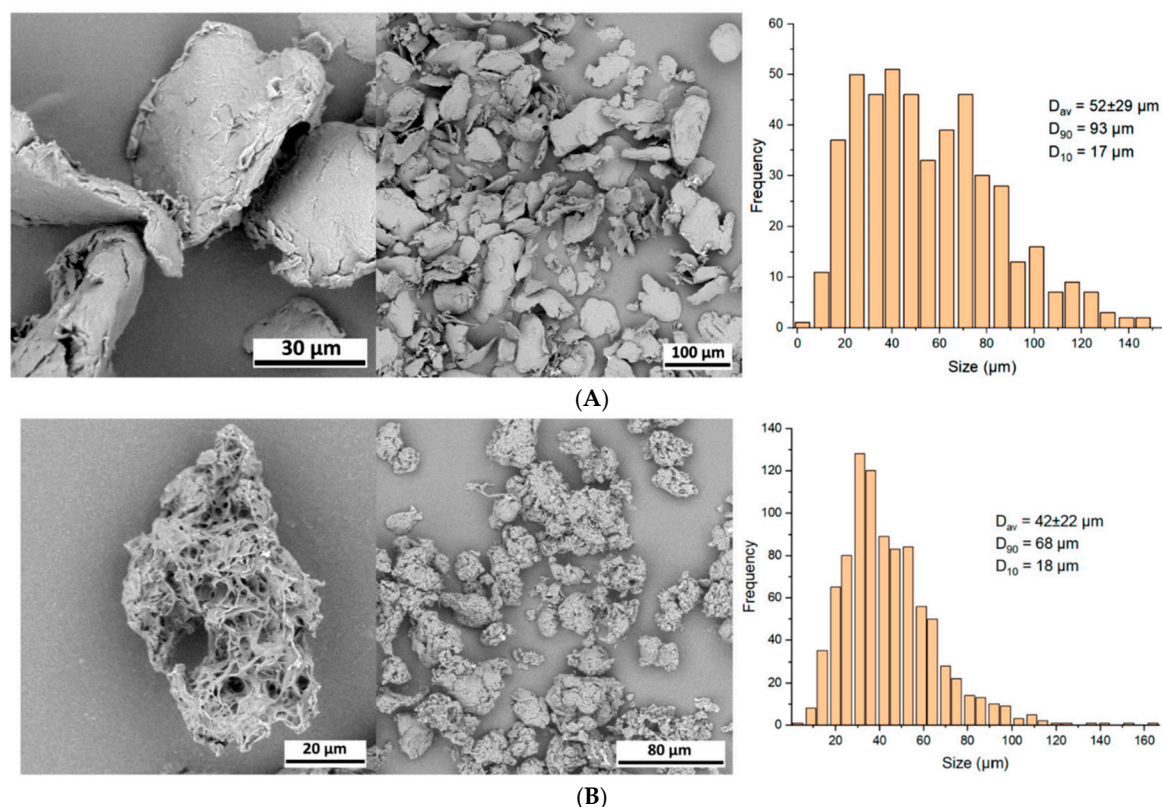


Figure 3. (A) Scanning electron microscopy at two magnifications and size distribution of reconstituted early-generation, irregular, plate-like PLLA microparticles (first example of currently available formulation). D_{av} = average diameter; D_{10} , D_{90} = tenth and ninetieth diameter percentiles. Credit: Ref. [18], figure republished under the terms of a Creative Commons CC BY-NC 4.0 License. (B) Scanning electron microscopy at two magnifications and size distribution of reconstituted early-generation, irregular, and highly porous PLLA microparticles (second example of currently available formulation). D_{av} = average diameter; D_{10} , D_{90} = tenth and ninetieth diameter percentiles. Credit: Ref. [18], figure republished under the terms of a Creative Commons CC BY-NC 4.0 License.

Conversely, the highly pure and readily dispersible microspheres of the innovative Class III JULÄINE™ medical device (Nordberg Medical AB, Huddinge, Sweden), produced using proprietary patented freeze-drying technologies, exhibit precise spherical shapes and smooth surfaces with a non-porous structure. They possess a uniform diameter ranging from 20 to 50 μm (average: 33.3 μm) and exhibit a consistent *in vivo* degradation rate over two years, along with long-term stability and shelf life (Figure 4) [21]. Each JULÄINE™ vial of dry powder contains 150 mg of PLLA-LASYNPRO™ microspheres; additional components include 45 mg of sodium carboxymethyl cellulose and 145 mg of non-pyrogenic mannitol [21]. Moisture and pro-inflammatory heavy metal and tin residues are below 0.5%, 0.001%, and 6.0 μg/mL (ppm), respectively, significantly lower than the levels found in earlier-generation PLLA derivatives [21].

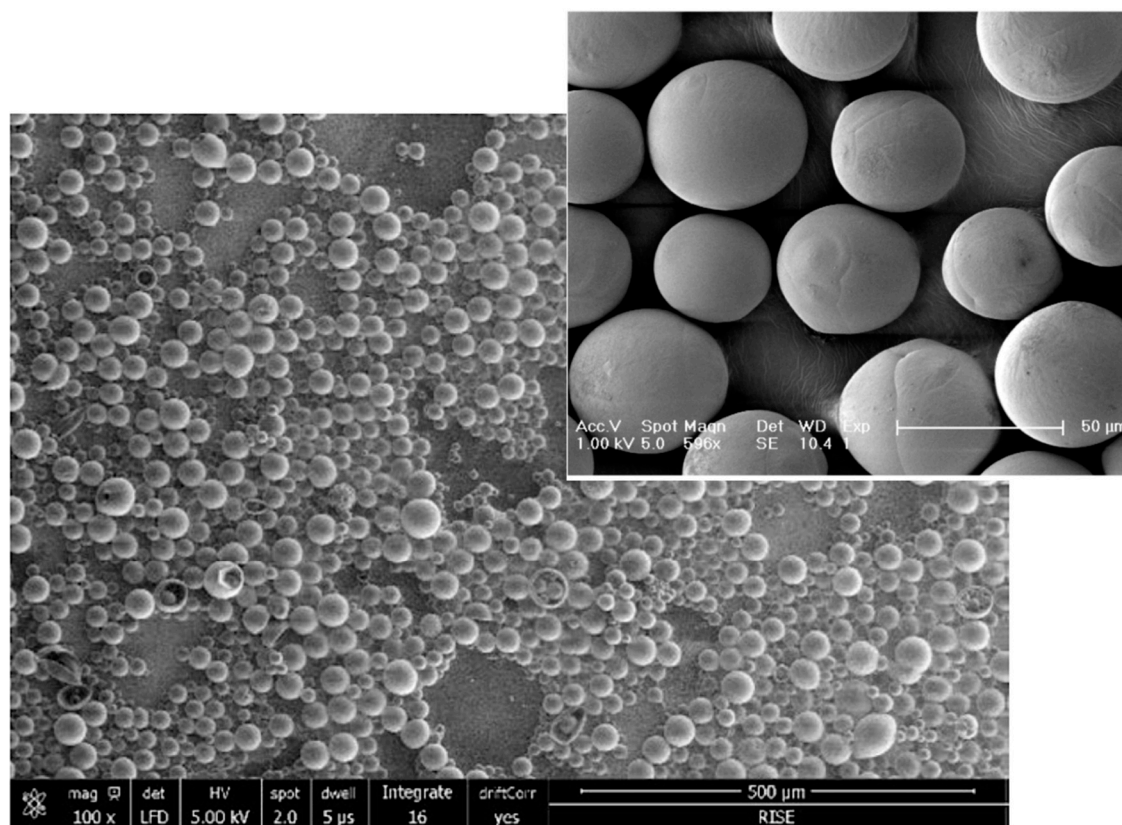


Figure 4. Scanning electron microscopy of PLLA-LASYNPRO™ microspheres at X100 (larger image) and X500 (upper-right detail) magnifications [21]. Credit: Nordberg Medical SA (R&D), Huddinge, Sweden, with agreement to publish.

The Non-Inflammatory Action of the New-Technology Microspheres

Even with earlier-generation PLLA formulations, the FBR paradigm does not fully explain collagen and extracellular matrix neosynthesis. For instance, the purely inflammatory FBR model does not clarify why a noticeable facial tightening effect often occurs just one month after earlier-generation PLLA injections, as the temporal framework seems too short [22].

In vitro evidence may provide a basis for elucidating the early tightening effects observed in vivo from earlier-generation PLLA formulations. For example, exposing fibroblasts to these conventional PLLA formulations for 48 hours activates the p38, Akt (protein kinase B), and JNK (c-Jun N-terminal kinase) signaling proteins, which are key regulators in signal transduction related to cell growth, differentiation, and apoptosis. This exposure also elevates the expression of the Type-I collagen gene [23]. The Akt signaling pathway contributes to fibroblast migration, differentiation into myofibroblasts, collagen synthesis, and cutaneous wound contraction. Gene transcription increases rapidly within 48 hours and is likely independent of any FBR-like effects. Following the upregulation of Type-I collagen gene expression, procollagen concentrations also rise quickly in the incubation medium [23].

Another well-known FBR-independent regenerative sequence of events that leads to collagen and ECM neosynthesis involves the pH-dependent activation of latent TGF- β (Transforming Growth Factor- β). Acidic lactate, produced by the gradual degradation of PLLA, triggers the regenerative signal [24,25]. Furthermore, active TGF- β directs fibroblasts to adopt the contractile myocyte phenotype, differentiate into myofibroblasts, and enhance the production of extracellular collagen and matrix. Additionally, active TGF- β prompts fibroblasts and myofibroblasts to upregulate the lactate-generating enzyme LDHA (lactate dehydrogenase-A), resulting in persistently high lactate concentrations and continuous local TGF- β activation [24–27]. *In vitro*, upregulation of the TIMP1

(Tissue Inhibitor of MetalloProteinase 1) signaling pathway by lactic acid represents a third TGF- β -triggered event, ultimately leading to sustained inhibition of collagen catabolism [28,29].

All such non-inflammatory events appear strongly activated by PLLA-LASYNPRO™ subdermal implants [22]. Furthermore, the gradual degradation of the new-technology PLLA microspheres into lactate monomers supports cellular energy production through the tricarboxylic acid cycle and the electron transport chain [30]. Figure 5 summarizes the likely *in vivo* effects on fibroblasts in dermal and subcutaneous connective tissues following exposure to the lactic acid monomers gradually released from the PLLA-LASYNPRO™ microspheres over several months. The activation of TGF- β by the acidic microenvironment induced by the lactate residues released from the microspheres promotes myofibroblast differentiation, collagen synthesis, and the formation of the extracellular matrix while reducing collagen degradation with minimal inflammatory responses (Figures 6A and 6B) [20,32–34]. The negligible inflammatory response, with no scar-like tissues or nodules and even dispersion without focal aggregations of the steadily and slowly degrading new-technology PLLA microspheres, persists for 24 months. There are no tissue compressions or deformities. Some microspheres remain detectable at month 18, with complete degradation occurring by month 24, leaving no residue or tissue gaps after degradation (Figure 7) [13,21]. The positive feedback loop would wane with the resorption of the microspheres, thus eliminating any long-term risk of fibrosis. The stimulating role of lactate on fibroblast collagen proline hydroxylase may also promote self-sustaining neocollagenesis [34,35]. The increased levels of IL-4 and IL-13 led to macrophage polarization toward the M2 subtype and tissue remodeling, further enhancing TGF- β secretion [31].

Moreover, recent *in vitro* studies with cultured adipocytes suggest that PLLA monomers may help stimulate adipogenesis in subcutaneous adipose tissues, potentially countering the loss of subcutaneous fat due to aging and photoaging, possibly contributing to deep wrinkles [37]. In general, PLLA monomers are more and more emerging as crucial signaling factors in the cell machinery. For instance, in skin fibroblasts, L-lactate protects mitochondria from aging-related dysfunction. Mito-hormesis, the name of the modulation process, is a persistent cellular adaptive response of mitochondria and mitochondria-associated membranes to mild stressors whereby skin fibroblasts enhance their survival and stress resistance, possibly by inducing the release of stress-triggered mitokines Fibroblast Growth Factor 21 (FGF21) and Growth and Differentiation Factor 15 (GDF15) [38].

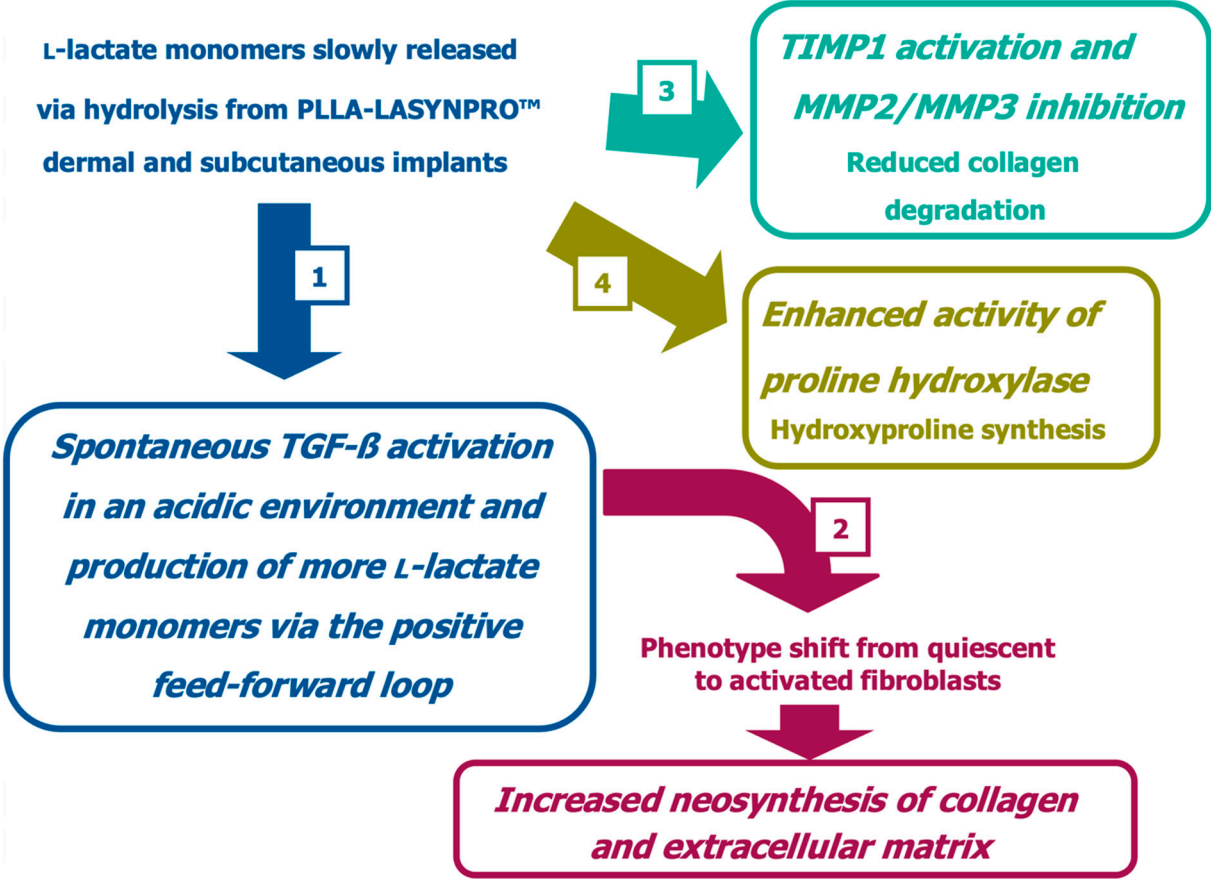
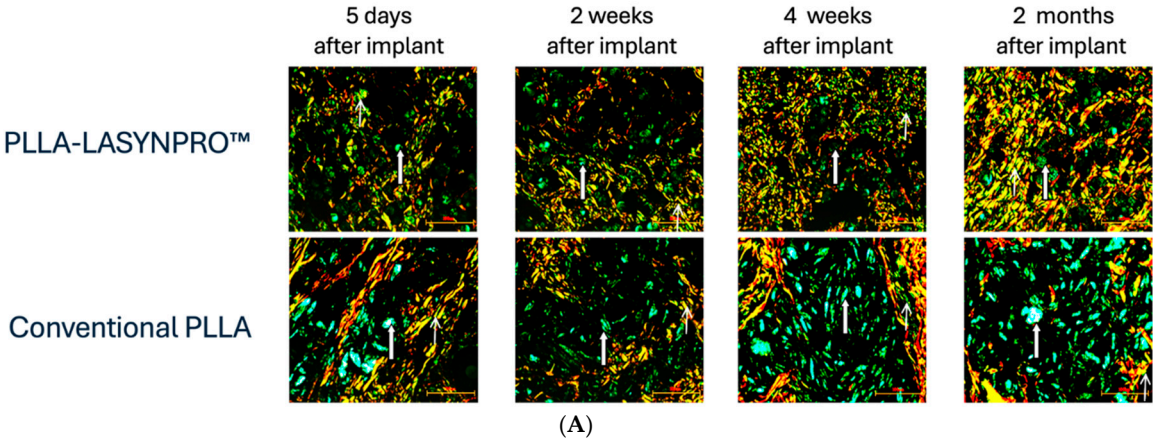


Figure 5. The non-inflammatory chain of events leading to neosynthesis of collagen and extracellular matrix: (1) Self-sustaining positive feed-forward loop of lactate-dependent TGF- β activation, sparked by the slow release of lactic acid monomers from PLLA-LASYNPRO™ implants and persistently supported over time by TGF- β -dependent lactate dehydrogenase (LDHA) upregulation (TGF- β : Transforming Growth Factor- β); (2) TGF- β -dependent conversion of quiescent fibroblasts into actively collagen-producing contractile myofibroblasts; (3) Concomitant inhibition of extracellular collagen degradation by lactic acid monomers (TIMP1: Tissue Inhibitor of Metalloproteinase 1); (4) The potential supportive role of lactic acid residues in stimulating proline hydroxylase leads to the expansion of the dermal and subcutaneous pool of the collagen-specific hydroxyproline amino acid. Diagram drawn and owned by the authors based on information from Ref. [31–36].



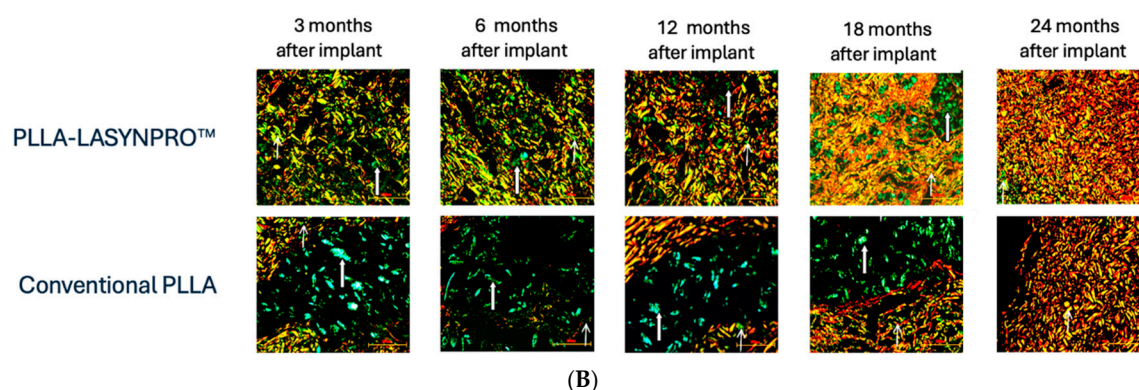


Figure 6. A. PLLA-LASYNPRO™ (upper row, international brand JULÄINE™, LÖVISELLE in the People's Republic of China): Intense deposition of collagen (Type-III fibers shown in yellow; Type-I fibers in red) and extracellular matrix begins and increases after the fourth week around the dispersed subdermal new-technology microspheres (green staining and arrows), with no signs of aggregation. Conventional PLLA (commercial earlier-generation PLLA formulation): sparse and irregular Type-III and Type-I neocollagenesis around persistent PLLA aggregates. Comparative evolution over the first two months (Picrosirius Red staining in lab models, X100 magnification) [13,21]. Credit: Nordberg Medical SA (R&D), Huddinge, Sweden, with agreement to publish. **B.** PLLA-LASYNPRO™ (upper row, international brand JULÄINE™, LÖVISELLE in the People's Republic of China): increasingly dense and regular deposition of collagen and extracellular matrix (Type-III fibers shown in yellow; Type-I fibers in red), transitioning over one year to a progressive prevalence of definitive Type-I fibers. The resorption of the PLLA-LASYNPRO™ microspheres (indicated by green staining and arrows) is nearly complete after two years, while the regular texture of newly deposited collagen fibers persists. Earlier-generation conventional PLLA: disorganized neocollagenesis at all times with slow degradation of PLLA microparticles and aggregates and, at 24 months, sparse surviving PLLA microparticles (arrow). The fibrous capsules surrounding hollow areas correspond to the resorbed earlier-generation PLLA microparticles. Comparative evolution from the third month to two years (Picrosirius Red staining in lab models, X100 magnification) [13,21]. Credit: Nordberg Medical SA (R&D), Huddinge, Sweden, with agreement to publish.

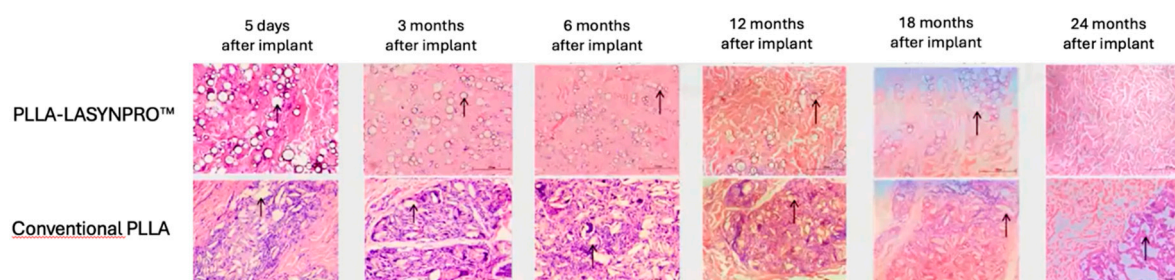


Figure 7. PLLA-LASYNPRO™ (upper row, international brand JULÄINE™, LÖVISELLE in the People's Republic of China): Negligible inflammation over 24 months. The microspheres do not aggregate, remain detectable after 18 months, and wane entirely after 24 months, leaving no gaps in tissues that maintain their orderly structure. Conventional PLLA (commercial earlier-generation PLLA formulation): Irregular neocollagenesis with disruption of the orderly subdermal histology surrounding persistent PLLA aggregates. Gaps and tissue hollows are detectable after 18 and 24 months (hematoxylin and eosin staining in lab models, X100 magnification) [13,21]. Credit: Nordberg Medical SA (R&D), Huddinge, Sweden, with agreement to publish.

Conclusions

Technological innovations have led to the novel PLLA-LASYNPRO™ subdermal implants. Are these implants a genuine breakthrough in addressing the inflammatory foreign-body response paradigm? We know from the past that some degree of inflammation has consistently accompanied the action of resorbable collagen inducers before the new-technology PLLA derivative [1].

As discussed in Part 2 of this introduction to PLLA-LASYNPRO™ non-inflammatory collagen and extracellular matrix regeneration, the Next-Generation PLLA-LASYNPRO™ Regenerative Medicine Expert Board cautiously endorsed the non-inflammatory rationale behind the new medical device [17]. They found the initial findings from preclinical and microscopic investigations [10,21–36] persuasive and aligned with their clinical experience as leaders in the ongoing clinical research program of the new PLLA technology. Their initial impression is that the CE-approved JULÄINE medical device, based on novel PLLA technology, may effectively address the challenge of inflammatory side effects [17]. In this context, the Next-Generation PLLA-LASYNPRO™ Regenerative Medicine Expert Board expressed the opinion that the new PLLA technology might indeed emerge as a breakthrough in skin regeneration without no more than mild and transitory inflammation. Caution and further research efforts remain essential in this initial phase to substantiate the first favorable results.

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Institutional Review Board Statement: No board activities involved interactions with human subjects, thus waiving the need for formal preliminary Institutional Review Board approval.

Informed Consent Statement: Not relevant.

Data Availability Statement: Minutes from the discussion at the final board meeting are available upon reasonable request.

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Conflicts of Interest: Over the past three years, all board members have received grants and fees from companies involved in aesthetic medicine and surgery, serving as consultants in research and development programs, investigators in national and international clinical studies, and lecturers or tutors in Continuous Medical Education activities and sponsored educational meetings. However, the authors declare no conflicts of interest related to the manuscript submission. Nordberg Medical AG, the holder of the international patents for PLLA-LASYNPRO™ and the manufacturer and exclusive marketer of the JULÄINE™ medical device, provided support only for the secretarial and logistical expenses of the board members and will also financially assist with publication costs after the manuscript undergoes peer review and acceptance.

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