

1 Article

2 **Enhanced nanoencapsulation of sepiapterin within**  
3 **PEG-PCL nanoparticles by complexation with**  
4 **triacetyl-beta cyclodextrin**5  
6 Nataliya Kuplennik and Alejandro Sosnik<sup>1,\*</sup>7  
8 <sup>1</sup> Laboratory of Pharmaceutical Nanomaterials Science, Department of Materials Science and Engineering,  
9 Technion-Israel Institute of Technology, Haifa, Israel10 \* Correspondence: Laboratory of Pharmaceutical Nanomaterials Science, De-Jur Bldg., Office 607,  
11 Department of Materials Science and Engineering, Technion-Israel Institute of Technology, 3200003 Haifa,  
12 Israel; Email: [sosnik@technion.ac.il](mailto:sosnik@technion.ac.il), [alesosnik@gmail.com](mailto:alesosnik@gmail.com); Tel.: +972-(0)77-887-197113  
14 Received: date; Accepted: date; Published: date  
1516 **Abstract:** In this work, we investigated for the first time the complexation of sepiapterin (SP), the  
17 natural precursor of the natural essential cofactor tetrahydrobiopterin, that displays mild water-  
18 solubility and short biological half-life, with the hydrophobic triacetyl- $\beta$ -cyclodextrin (TA $\beta$ CD) to  
19 improve its encapsulation within methoxy-poly(ethylene-glycol)-poly(epsilon-caprolactone)  
20 (mPEG-PCL) nanoparticles. First, TA $\beta$ CD-SP complexes were produced by spray-drying of  
21 TA $\beta$ CD/SP binary solutions by utilizing the Nano Spray Dryer B-90 HP. Then, dry powders were  
22 characterized by differential scanning calorimetry (DSC), Fourier-transform infrared spectroscopy  
23 (FTIR) and transmission and scanning electron microscopy (SEM and TEM, respectively) and  
24 compared to the complex components and physical mixtures (PMs). Next, SP was encapsulated  
25 within methoxy-poly(ethylene-glycol)-poly(epsilon-caprolactone) (mPEG-PCL) nanoparticles by  
26 nanoprecipitation of a SP/TA $\beta$ CD complex/mPEG-PCL solution. In addition to complex  
27 nanoencapsulation, we assessed encapsulation of pure SP by nanoprecipitation with an  
28 intermediate step, which comprised the co-drying of SP, TA $\beta$ CD and mPEG-PCL copolymer  
29 solution in organic solvent; this step aimed to promote the formation of molecular interactions  
30 between SP, TA $\beta$ CD and the PCL blocks in the copolymer. SP-loaded mPEG-PCL nanoparticles  
31 were characterized by dynamic light scattering (DLS) and SEM. Nanoparticles with size of 74-75 nm  
32 and small polydispersity index (PDI <0.1) were obtained when SP-TA $\beta$ CD equimolar spray-dried  
33 complex was used for nanoencapsulation, and SEM analysis indicated the absence of free SP  
34 crystals. Moreover, the encapsulation efficiency (%EE) and drug loading (DL) were 85% and 2.6%,  
35 respectively, as opposed to those achieved with pure SP encapsulation (14% and 0.6%, respectively).  
36 Overall, our results confirm that spray-drying of SP/TA $\beta$ CD solutions at the appropriate molar ratio  
37 leads to the hydrophobization of the relatively hydrophilic SP molecule, enabling its encapsulation  
38 within mPEG-PCL nanoparticles.  
3940 **Keywords:** Sepiapterin; triacetyl- $\beta$ -cyclodextrin (TA $\beta$ CD); hydrophilic drug/cyclodextrin complexes;  
41 spray-drying; methoxy-poly(ethylene-glycol)-poly(epsilon-caprolactone) (mPEG-PCL)  
42 nanoparticles.  
4344 **1. Introduction**45 Tetrahydrobiopterin (BH<sub>4</sub>, **Figure S1**), a naturally occurring molecule, is present in probably  
46 every cell or tissue of higher organisms and it is well-established as cofactor in various essential

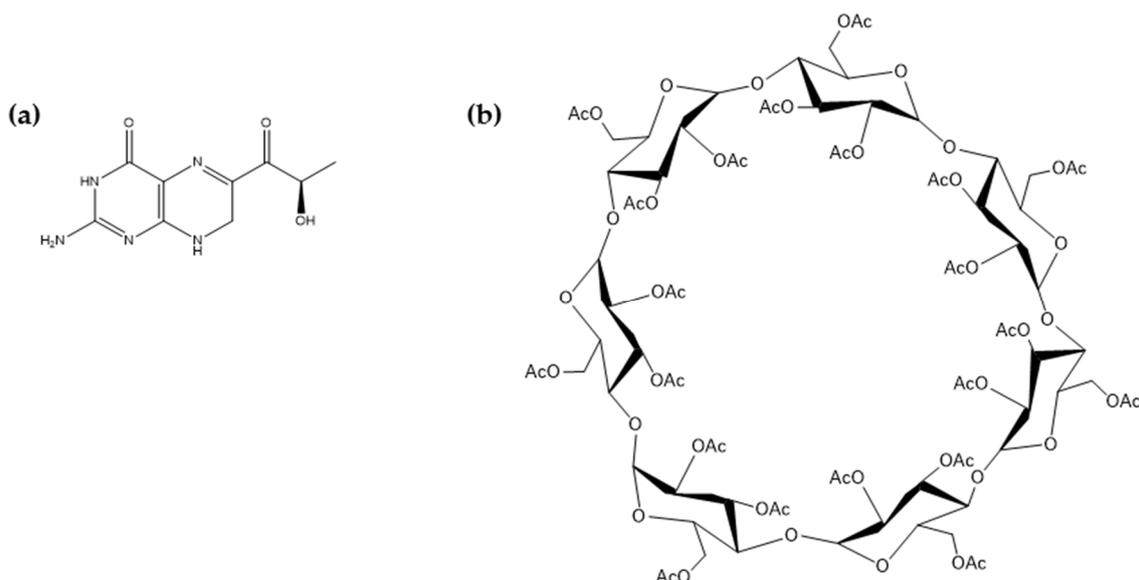
47 enzymatic pathways that include the degradation of phenylalanine and the biosynthesis of  
48 neurotransmitters such as serotonin, melatonin, dopamine, noradrenaline and adrenaline [1,2]. BH4  
49 is also a key player in various biological processes associated with cardiovascular homeostasis and  
50 the immune response [1,3]. Defects in BH4 metabolism caused by congenital mutations in specific  
51 genes encoding for enzymes involved in its synthesis or regeneration and known with the general  
52 name of BH4 deficiency lead to the systemic deficiency of neurotransmitters in the CNS [4].  
53 Moreover, decreased levels of BH4 have been also documented in neurological diseases such as  
54 Parkinson's disease, autism, depression and Alzheimer's disease. In some of them, administration of  
55 BH4 has been reported to improve the clinical symptoms [1,5]. However, BH4 undergoes fast aerobic  
56 degradation, which results in a decrease of the treatment efficacy [6]. BH4 deficiency is a disease with  
57 severe impact on neurological and cognitive development. In this framework, the development of  
58 advanced delivery systems that improve the biological half-life of BH4 and its bioavailability in the  
59 central nervous system (CNS) emerges as a strategy to enhance the efficacy of the current replacement  
60 therapy.

61 There exists a broad spectrum of synthetic biodegradable polymers used for production of  
62 nanoparticulate drug delivery systems that improve the physicochemical stability and sustain the  
63 release of hydrophobic cargos [7]. Among them, block copolymers made of hydrophilic components  
64 (e.g., poly(ethylene glycol), PEG) and hydrophobic polyester blocks such as poly(lactic acid) (PLA),  
65 poly(lactic-co-glycolic acid) (PLGA) and poly(epsilon-caprolactone) (PCL) have gained major  
66 attention owing to the ability to fine-tune the hydrophilicity/lipophilicity and the thermal properties  
67 of the product and consequently to control the biodegradation and the release of the cargo in the  
68 biological environment [8–15]. However, BH4 is highly water-soluble ( $S_0 = 23 \text{ mg ml}^{-1}$ ) and extremely  
69 instable in water and air (**Figure S2**), precluding its encapsulation within polymeric nanoparticles.

70 Sepiapterin (SP, **Figure 1a**) is the natural precursor of BH4 and it is intracellularly converted into  
71 BH4 [16]. SP displays lower aqueous solubility ( $1.7 \text{ mg ml}^{-1}$ ) and higher chemical stability than BH4  
72 and thus, it appears a good candidate to replace it in the design of advanced drug delivery systems.  
73 At the same time, encapsulation of relatively hydrophilic molecules within hydrophobic polymeric  
74 nanoparticles by utilizing conventional preparation methods remains a challenge and the  
75 development of new encapsulation procedures is called for [17,18].

76 The use of cyclodextrins to increase the aqueous solubility of hydrophobic drugs has been  
77 extensively investigated [19–22]. Recently, peracylated cyclodextrins (CDs) that are freely soluble in  
78 organic solvents and poorly water-soluble were proposed as excipients to decrease the water-  
79 solubility, prolong the biological half-life and sustain the release of hydrophilic drugs through the  
80 synthesis of water insoluble drug/CD complexes [23–27].

81 Aiming to encapsulate SP within polymeric nanoparticles as a platform for delivery and  
82 targeting, in this work, we synthesized for the first time a SP/triacetyl- $\beta$ -cyclodextrin (TA $\beta$ CD)  
83 (**Figure 1b**) complex by spray-drying SP/TA $\beta$ CD binary solutions utilizing the Nano Spray Dryer B-  
84 90 HP. Then, dry powders were characterized by differential scanning calorimetry (DSC), Fourier-  
85 transform infrared spectroscopy (FTIR) and transmission and scanning electron microscopy (SEM  
86 and TEM, respectively) and compared to the pure complex components and SP/CD physical mixtures  
87 (PMs). Finally, the optimized complex was encapsulated within methoxy-poly(ethylene-glycol)-  
88 poly(epsilon-caprolactone) (mPEG-PCL) nanoparticles by a direct nanoprecipitation method. Overall  
89 results confirm the promise of this simple and scalable strategy for the nanoencapsulation of SP.



**Figure 1.** Chemical structure of (a) SP and (b) TA $\beta$ CD.

90  
91  
92

## 93 2. Results and Discussion

### 94 2.1. BH4 and SP stability

95 BH4 (**Figure S1**) is known to undergo rapid degradation. Due to oxidation, BH4 solution  
96 becomes yellow. SP is known to be less sensitive to oxygen than BH4. The stability of BH4 and SP in  
97 deionized oxygen-free water (1% w/v) was investigated by UV/Vis spectrophotometry (**Figure**  
98 **S2**). The absorbance peak of BH4 at 266 nm decreased by 15% and red-shifted after 48 h, while a new  
99 absorbance peak at 329 nm appeared already after 1 h (**Figure S2a**). This also results in a change color  
100 to yellow. Conversely, SP remained stable even after 8 days, confirming that this precursor is much  
101 more stable than BH4 and a better candidate for encapsulation (**Figure S2b**). Moreover, the intrinsic  
102 solubility of BH4 in water is higher than of SP and thus, its encapsulation in hydrophobic polymers  
103 precluded. Thus, SP was chosen for further experiments, both due to higher stability and lower  
104 solubility.

105 For improvement of SP encapsulation within mPEG-PCL nanoparticles, we assessed two  
106 approaches: (i) drying of a solution of SP, TA $\beta$ CD and mPEG-PCL copolymer in acetone prior to  
107 redissolution in acetone and nanoprecipitation and (ii) spray-drying of a solution of SP and TA $\beta$ CD  
108 to obtain SP-TA $\beta$ CD complex, and subsequent nanoprecipitation of the complexes and copolymers  
109 to obtain SP-encapsulated nanoparticles. Nanoprecipitation in both approaches was performed  
110 according to the protocol described in the experimental section. Spray-dried SP/TA $\beta$ CD complexes  
111 were further fully characterized to get an insight on interactions occurring between the two  
112 components.

### 113 2.2. Characterization of spray-dried SP/TA $\beta$ CD complexes

114 In order to investigate possible SP/TA $\beta$ CD interactions and exclude artifacts resulting from the  
115 sample preparation, pure TA $\beta$ CD was subjected to the same procedure (dissolution and spray-  
116 drying) as binary SP/TA $\beta$ CD solutions; this sample is named processed TA $\beta$ CD. Pure SP was not  
117 spray-dried owing to its high cost as spray-drying requires relatively large amounts for sample  
118 collection. Instead, a reference sample (processed SP) was prepared by dissolution of SP in ethanol  
119 and drying under vacuum. Two SP:TA $\beta$ CD molar ratios were used for complex preparation:  
120 equimolar (1:1) and with an excess of TA $\beta$ CD (2:1) (**Table 1**). PMs of the pure components with the  
121 same molar ratios were prepared by grinding of dry TA $\beta$ CD and SP using mortar and pestle.

122

123

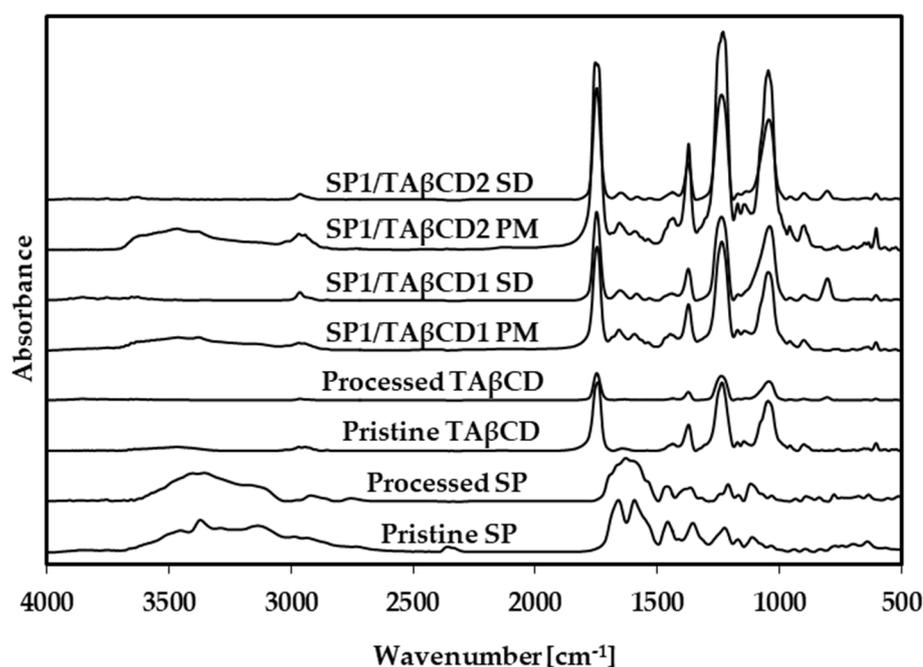
**Table 1.** Nomenclature of SP/TA $\beta$ CD complexes and their PMs.

Preparation method	SP:TA $\beta$ CD molar ratio	Nomenclature
Spray-drying (SD)	1:1	SP1/TA $\beta$ CD1 SD
	1:2	SP1/TA $\beta$ CD2 SD
Drying with copolymer (DWC)	1:1	SP1/TA $\beta$ CD1 DWC
	1:2	SP1/TA $\beta$ CD2 DWC
Physical mixture (PM)	1:1	SP1/TA $\beta$ CD1 PM
	1:2	SP1/TA $\beta$ CD2 PM

124

125 *2.2.1. Fourier-transform infrared spectroscopy*

126 FTIR spectra of SP, TA $\beta$ CD, their PMs and the spray-dried samples are shown in **Figure 1**. Pure  
 127 and processed SP showed two bands at 3444 and 3377 cm<sup>-1</sup> of N–H stretching vibration of primary  
 128 amine, a band at 3155 cm<sup>-1</sup> due to the N–H stretching of secondary amine, and characteristic bands  
 129 at 1620 and 1590 cm<sup>-1</sup> assigned to N–H bending of primary amine (**Figure 1**). TA $\beta$ CD displayed very  
 130 strong bands at 1708, 1371, 1234 and 1045 cm<sup>-1</sup> that correspond to C=O, -CH<sub>3</sub> and C–O–C vibrations  
 131 of the acetyl group (**Figure 1**) [28]. PMs spectra showed the overlapping of the bands of pure SP and  
 132 TA $\beta$ CD and no significant shifts or depletion of the intensity of the characteristic bands with respect  
 133 to the pure components were observed. In contrast, FTIR spectra of the spray-dried SP/TA $\beta$ CD  
 134 revealed a strong reduction or the complete disappearance of the characteristic SP bands in the 3800–  
 135 3000 cm<sup>-1</sup> region, suggesting the interaction between SP and TA $\beta$ CD and the formation of a complex.  
 136

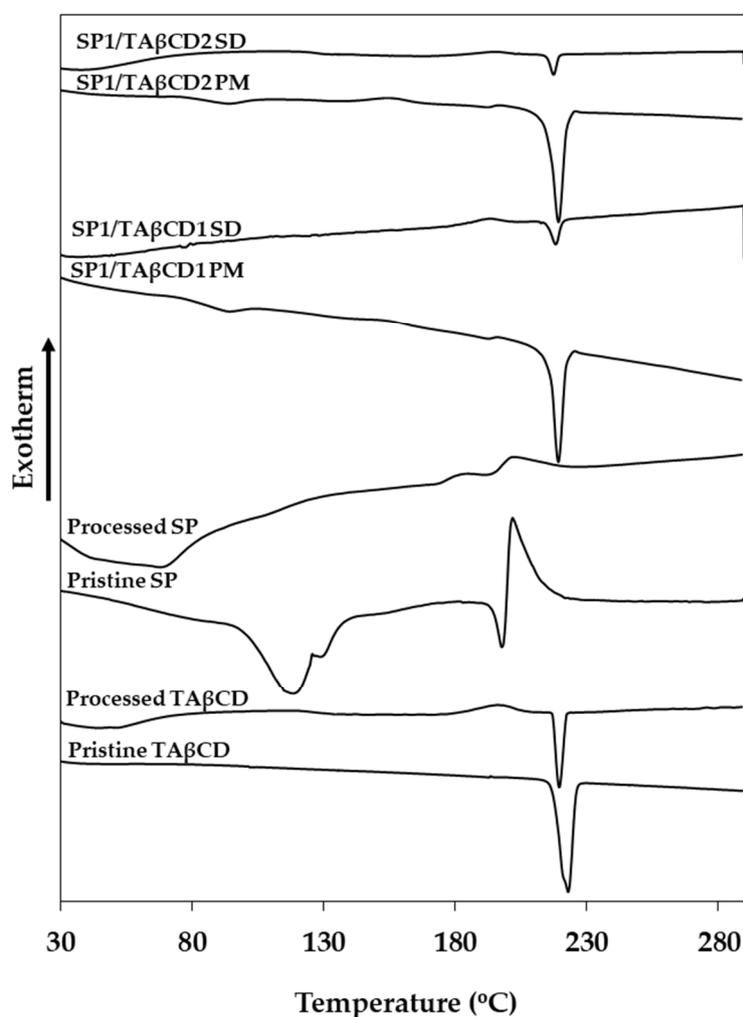


137 **Figure 1.** FTIR spectra of pristine and processed SP and TA $\beta$ CD, their PMs and the SP/TA $\beta$ CD  
 138 complexes obtained by spray-drying.

139 *2.2.2. Differential scanning calorimetry (DSC)*

140 DSC is widely used to study the interaction between a drug and a CD in the solid state  
 141 [20,29,30]. Thus, to further confirm the formation of a complex, we compared the thermal behavior  
 142 of pristine SP, SP/TA $\beta$ CD PMs and spray-dried SP/TA $\beta$ CD by DSC. Pristine TA $\beta$ CD was

143 characterized by a sharp melting endotherm at 223°C (**Figure 2**) associated with a melting enthalpy  
 144 ( $\Delta H_m$ ) of 7.13 J g<sup>-1</sup> (**Table 2**). Processed TA $\beta$ CD thermal behavior differed from the pristine one; spray-  
 145 dried TA $\beta$ CD displayed an exothermic peak upon heating at 195°C due to the crystallization of  
 146 amorphous TA $\beta$ CD with a crystallization enthalpy ( $\Delta H_c$ ) of 8.4 J g<sup>-1</sup> (**Figure 2**). The recrystallization  
 147 of acetylated CDs that undergo amorphization during spray-drying was described elsewhere [31].  
 148 Then, recrystallized TA $\beta$ CD melted at 220°C, though a smaller  $\Delta H_m$  of 13 J g<sup>-1</sup> than in pristine TA $\beta$ CD  
 149 (43 J g<sup>-1</sup>) was observed (**Table 2**). This kind of behavior was also reported for TA $\beta$ CD recrystallized  
 150 from water/organic solvent solutions and indicates the partial amorphization of the CD [31]. Pure SP  
 151 showed a more complex thermal behavior. A broad endotherm at 116°C ( $\Delta H_m = 77.3$  J g<sup>-1</sup>) probably  
 152 stemmed from the release of bound water (**Figure 2, Table 2**). Then, the beginning of melting was  
 153 observed at 190°C followed by decomposition. Processed SP showed a similar profile, though the  
 154 water-related peak of pristine SP was not apparent in the processed counterpart, suggesting the  
 155 efficient elimination of water residues available in the original sample. However, the broad  
 156 endotherm at 69°C probably corresponded to the evaporation of some solvent residues.  
 157



158

159 **Figure 2.** DSC thermograms of pristine and processed SP and TA $\beta$ CD, their PMs and the complexes  
 160 obtained by spray-drying.

161 The thermal analysis of PMs presented the endotherm associated with water release and the  
 162 characteristic transitions of pure SP and TA $\beta$ CD. TA $\beta$ CD crystallization on heating at lower  
 163 temperatures resulted from recrystallization of an amorphous form, obtained during the grinding  
 164 in the preparation of PMs [26]. Appearance of weak endothermic peak at 190°C, followed by an

165 exotherm, similar to that of pristine SP, was observed in both SP1/TA $\beta$ CD1 and SP1/TA $\beta$ CD2 PMs.  
 166 However, due to relatively low weight fraction of SP in the samples, these peaks were less prominent  
 167 compared to pristine SP. Such kind of thermal behavior of a drug in binary drug/CD PMs is typical  
 168 of this kind of systems [32,33]. These observations suggest that there are no solid-state interactions  
 169 between the two components in the PM. In contrast, DSC curves of the spray-dried SP/TA $\beta$ CD  
 170 complexes showed complete disappearance of the SP melting peak, and a strong reduction in the  
 171  $\Delta H_m$  of TA $\beta$ CD, indicating the total SP and the partial TA $\beta$ CD amorphization, and the formation of  
 172 a SP/TA $\beta$ CD complex. In addition, considering that SP is a relatively hydrophilic molecule and that  
 173 the cavity of TA $\beta$ CD is hydrophobic, it is likely that SP/TA $\beta$ CD form a non-inclusion complex.

174 **Table 2.** Thermal analysis of pristine and processed SP and TA $\beta$ CD, spray-dried complexes and  
 175 PMs, as determined by DSC. Enthalpy values were normalized to TA $\beta$ CD and SP content.

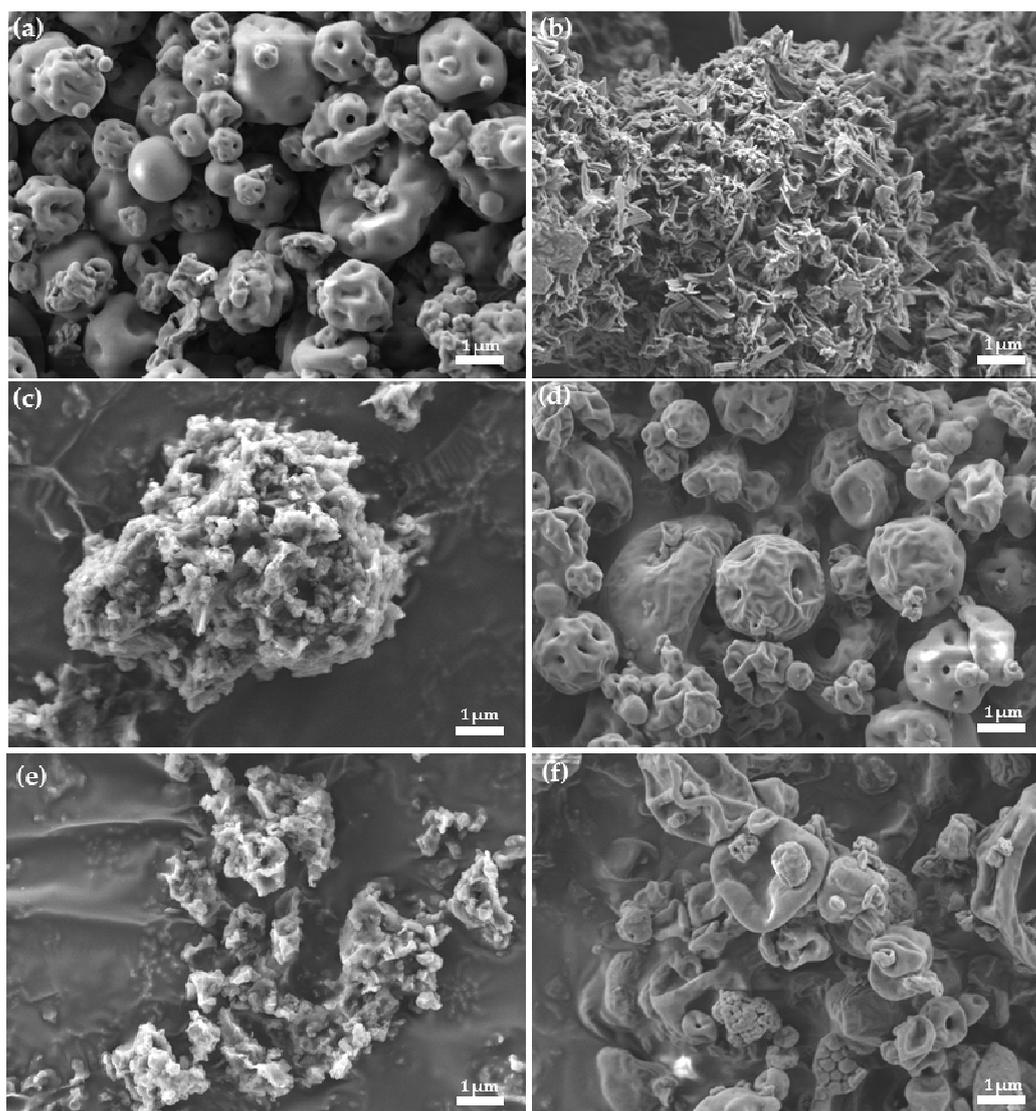
Sample	TA $\beta$ CD				SP	
	T <sub>m</sub> [°C]	$\Delta H_m$ [J g <sup>-1</sup> ]	T <sub>c</sub> [°C]	$\Delta H_c$ [J g <sup>-1</sup> ]	T <sub>m</sub> [°C]	$\Delta H_m$ [J g <sup>-1</sup> ]
Pristine TA $\beta$ CD	223	43	-	-	-	-
Processed TA $\beta$ CD	220	13	195	8.4	-	-
Pristine SP	-	-	-	-	190 (with decomposition)	-
Processed SP	-	-	-	-	-	-
SP1/TA $\beta$ CD1 SD	219	7.3	193	4.7	-	-
SP1/TA $\beta$ CD1 PM	219	40	153	3.2	-	-
SP1/TA $\beta$ CD2 SD	217	4.2	195	4.7	-	-
SP1/TA $\beta$ CD2 PM	219	43	155	5.6	-	-

176

### 177 2.2.3. Morphological characterization of spray-dried complexes

178 Morphological characterization of the drug/CD complexes by electron microscopy is widely  
 179 used [30,34]. Nevertheless, it should be mentioned that even if an apparent difference in  
 180 crystallization state of the raw materials compared to the products exists, this characterization  
 181 method should be used to confirm the formation of a complex only when combined with other  
 182 chemical and thermal characterization methods [32]. The surface aspect of processed SP and TA $\beta$ CD,  
 183 their PMs and the spray-dried complexes were visualized by HR-SEM (dry powders) and TEM  
 184 (powders re-suspended in water and casted). In HR-SEM, processed (spray-dried) TA $\beta$ CD appeared  
 185 as round-shaped amorphous particles (0.5-5  $\mu$ m) (**Figure 3a**). In addition, processed SP showed  
 186 irregular elongated needle-like crystals formed due to its crystallization during solvent evaporation.  
 187 HR-SEM micrographs of SP/TA $\beta$ CD PMs revealed the presence of the SP crystals dispersed in  
 188 TA $\beta$ CD (**Figure 3c,e**); no molecular interactions between the two substances in solid state were  
 189 observed. Conversely, spray-dried mixtures appeared as round-shape particles, similar to spray-  
 190 dried pristine TA $\beta$ CD, with no visible SP crystals (**Figure 3d,f**). These results were consistent with  
 191 DSC analysis and confirmed the amorphous nature of the spray-dried SP/TA $\beta$ CD binary systems.

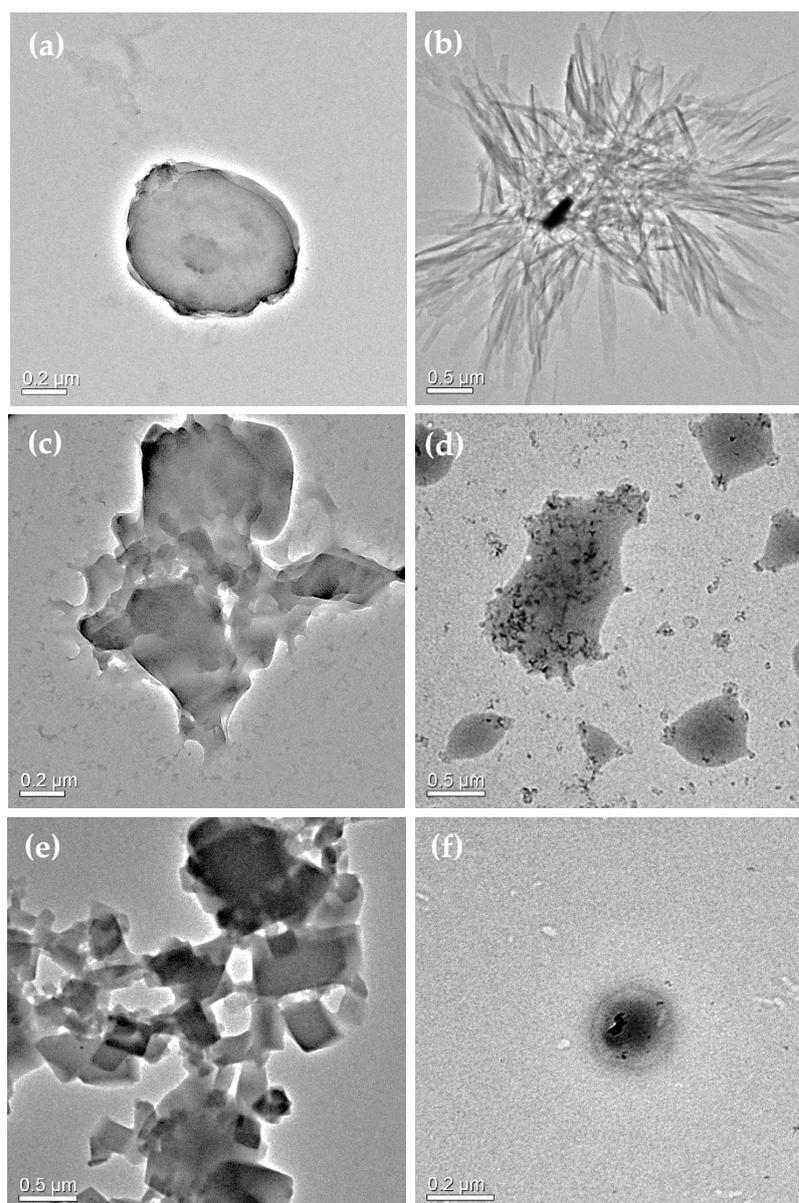
192



193 **Figure 3.** HR-SEM micrographs of (a) processed TAβCD, (b) processed SP, (c) SP1/TAβCD1 PM, (d)  
 194 spray-dried SP1/TAβCD1 complex, (e) SP1/TAβCD2 PM and (f) spray-dried SP1/TAβCD2 complex.

195 In addition, in TEM, processed TAβCD appeared as particles of irregular shape (**Figure 4a**),  
 196 while a processed SP sample produced by direct drop casting showed a needle-like crystalline  
 197 morphology (**Figure 4b**). These results were similar to those obtained in HR-SEM. Both SP/TAβCD  
 198 PMs showed the presence of square-shaped glassy chip structures that are typical for TAβCD (**Figure**  
 199 **4c,e**), while these structures were not observed in spray-ried complexes (**Figure 4d,f**) [31]. These  
 200 observations further supported that both components undergo amorphization during spray-drying.

201



202

203 **Figure 4.** TEM micrographs of (A) processed TAβCD, (B) processed SP, (C) SP1/TAβCD1 PM, (D)  
 204 spray-dried SP1/TAβCD1 complex, (E) SP1/TAβCD2 PM and (F) spray-dried SP1//TAβCD2 complex.

205 2.3. Production and characterization of SP-loaded nanoparticles

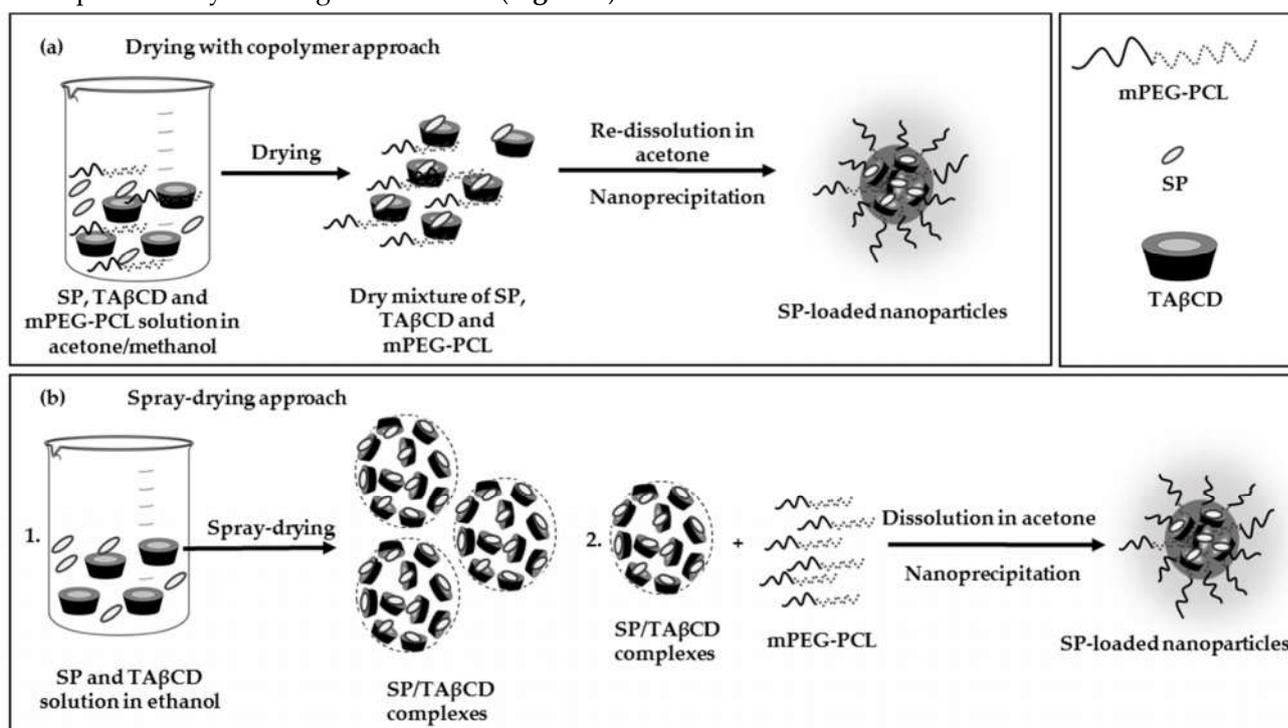
206 2.3.1. mPEG-PCL copolymer synthesis.

207 A mPEG-PCL copolymer with a relatively low hydrophilic-lipophilic balance was chosen as a  
 208 model for nanoparticle production and synthesized by the ring opening polymerization (ROP) of  
 209 epsilon-caprolactone (CL) initiated by the terminal hydroxyl group of a methoxy-terminated PEG  
 210 with a molecular weight of 4000 g mol<sup>-1</sup> in the presence of tin(II) 2-ethylhexanoate (SnOct) as catalyst  
 211 at 145°C for 2.5 h and in the appropriate CL:mPEG molar ratio to obtain a PCL block of approximately  
 212 20,000 g mol<sup>-1</sup> (**Figure S3**). The successful polymerization was confirmed by proton nuclear magnetic  
 213 resonance spectroscopy (<sup>1</sup>H-NMR) (**Figure S4**) and the number average molecular weight ( $M_n$ ), the  
 214 weight average molecular weight ( $M_w$ ) and the dispersity ( $D$ ,  $M_w/M_n$ ) of the copolymer measured by  
 215 gel permeation chromatography (GPC) (**Table S1**). **Figure S4** shows a representative <sup>1</sup>H-NMR  
 216 spectrum of the obtained mPEG-PCL copolymer. The peak at  $\delta = 3.60$  ppm was assigned to the

217 methylene ( $-\text{CH}_2$ ) protons of the PEG chain. In addition, characteristic peaks of the methylene  
 218 protons of the PCL block appeared at  $\delta = 2.26, 1.61, 1.35,$  and  $4.02$  ppm. Since the number-average  
 219 molecular weight of the PEG block used for the reaction is known from the supplier, the molecular  
 220 weight of PCL block was calculated by taking the integration ratio of the characteristic peak of PEG  
 221 ( $\delta = 3.60$  ppm) and PCL ( $\delta = 2.26$  ppm) (Table S1). In addition, the molecular weight of the copolymer  
 222 was measured by GPC (Table S1). The experimental molecular weight was similar to the theoretical  
 223 one.

### 224 2.3.2. Nanoencapsulation of SP.

225 Pristine SP was encapsulated within mPEG-PCL nanoparticles by a modified nanoprecipitation  
 226 method performed under inert nitrogen conditions in a flask protected from light to prevent the  
 227 possible oxidation of SP. Aiming to improve the SP loading within the nanoparticles, we assessed the  
 228 encapsulation by utilizing two methods (Figure 5).



229 **Figure 5.** Method for the encapsulation of SP. (a) Drying of the SP, TA $\beta$ CD with mPEG-PCL  
 230 copolymer prior to nanoprecipitation and (b) co-dissolution of spray-dried SP/TA $\beta$ CD complex with  
 231 the copolymer and nanoprecipitation.

232 The first included dissolution of SP, TA $\beta$ CD and the mPEG-PCL copolymer in organic solvent,  
 233 drying, and re-dissolving in acetone with subsequent nanoprecipitation and nanoparticle formation  
 234 (Figure 5a), while in the second, a spray-dried SP/TA $\beta$ CD complex was co-dissolved with the  
 235 copolymer and used for the nanoprecipitation (Figure 5b). It is worth stressing that equivalent  
 236 amounts of each component were used, as depicted in Table 3.

237

238

239

240

**Table 3.** Equivalent amounts of the different components used for the encapsulation of SP in mPEG-PCL nanoparticles.

Formulation	Equivalent amount used for encapsulation		
	mPEG-PCL [mg]	SP [mg]	TA $\beta$ CD [mg]
Pure SP		2	-
		1	-
SP1/TA $\beta$ CD1 DWC		2	17
		1	8.5
SP1/TA $\beta$ CD2 DWC	50	2	34
		1	17
SP1/TA $\beta$ CD1 SD		2	17
		1	8.5
SP1/TA $\beta$ CD2 SD		2	34
		1	17

As for the first approach of preliminar dissolution of all three components and drying, we aimed to promote both the interactions between hydrophobic TA $\beta$ CD and slightly more hydrophilic SP, as well as between hydrophobic PCL blocks of the copolymer and TA $\beta$ CD and thus, increase the entrapment of SP molecules in the PCL/TA $\beta$ CD matrix formed during the nanoprecipitation process with respect to TA $\beta$ CD-free counterparts.

### 2.3.3. Size and size distribution of SP-loaded nanoparticles.

The size (hydrodynamic diameter,  $D_h$ ) and size distribution (polydispersity index, PDI) of SP-free and SP-loaded nanoparticles produced by both methods, as well as suspensions of free TA $\beta$ CD subtracted to nanoprecipitation at the same conditions, were measured by DLS (**Table 4**).

**Table 4.** Characterization of SP-loaded mPEG-PCL nanoparticles: size and size distribution (as measured by DLS), SP encapsulation yield and drug loading in the nanoparticles.

Formulation	SP equivalent amount used for encapsulation [mg]	$D_h$ [nm]* ( $\pm$ S.D.)	%Intensity	PDI ( $\pm$ S.D.)	%EE [%] <sup>a</sup> ( $\pm$ SD)	DL [%] <sup>a</sup> ( $\pm$ SD)
TA $\beta$ CD	-	312 (25)	100	0.231 (0.076)	-	-
SP-free nanoparticles	-	65 (3)	100	0.155 (0.030)	-	-
Pure SP	1	73 (3)	100	0.130 (0.024)	9 (1)	0.2 (0.1)
	2	83 (2)	100	0.099 (0.022)	14 (1)	0.6 (0.1)
SP1/TA $\beta$ CD1 DWC	1	72 (7)	84	0.362 (0.069)	0 (0)	0 (0)
		353 (71)	16			
	2	100 (25)	86	0.419 (0.051)	11 (1)	0.4 (0.1)
		4260 (226)	14			
SP1/TA $\beta$ CD2 DWC	1	105 (5)	100	0.270 (0.037)	7 (1)	0.1 (0)
	2	99 (14)	77	0.749 (0.253)	9 (1)	0.3 (0)
		5066 (546)	23			
SP1/TA $\beta$ CD1 SD	1	74 (1)	100	0.094 (0.02)	62 (1)	1.1 (0.1)

	2	75 (2)	100	0.091 (0.021)	85 (1)	2.6 (0.1)
SP1/TAβCD2	2	69 (3)	51	0.694	53 (1)	0.9 (0.1)
SD		312 (35)	40	(0.067)		
		4071 (852)	9			
	1	72 (1)	89	0.389	50 (1)	1.5 (0.1)
		5105 (496)	11	(0.093)		

269 <sup>a</sup> Results are the average of 3 experiments (n = 3).

270

271 All the SP-loaded nanoparticles produced by the first approach, with the exception of the  
 272 SP1/TAβCD2 formulation that used 1 mg of SP, showed two size populations: one major in the  
 273 nanoscale (72-100 nm) and one minor in the microscale (4.2-5 μm) (**Table 4**). SP1/TAβCD2 DWC with  
 274 1 mg SP results in nanoparticles with monomodal size distribution and  $D_h$  of 105 nm. These results  
 275 indicated the poor mixing between both hydrophobic components in the nanoparticles. In the case of  
 276 spray-dried complexes, SP1/TAβCD1 resulted in nanoparticles with small size of 74-75 nm and PDI  
 277 <0.1 (**Table 4**).

#### 278 2.3.4. Encapsulation efficiency and drug loading.

279 Two parameters, the encapsulation efficiency (%EE) and the drug loading (DL) of SP in mPEG-  
 280 PCL nanoparticles were quantified. For this, SP-loaded nanoparticle suspensions were washed  
 281 thoroughly to remove residues of free TAβCD and SP, free SP quantified in the filtrate fraction and  
 282 the %EE calculated according to **Equation 1**

283

$$284 \quad \%EE = \frac{SP_{\text{nanoparticle}}}{SP_t} \times 100\% \quad (1)$$

285

286 Where  $SP_{\text{nanoparticle}}$  is the weight of SP in the nanoparticles and  $SP_t$  is the total weight of SP used in the  
 287 encapsulation process.

288

289 In addition, the DL was calculated according to **Equation 2**

290

$$291 \quad DL = \frac{SP_{\text{nanoparticle}}}{NP_t} \times 100\% \quad (2)$$

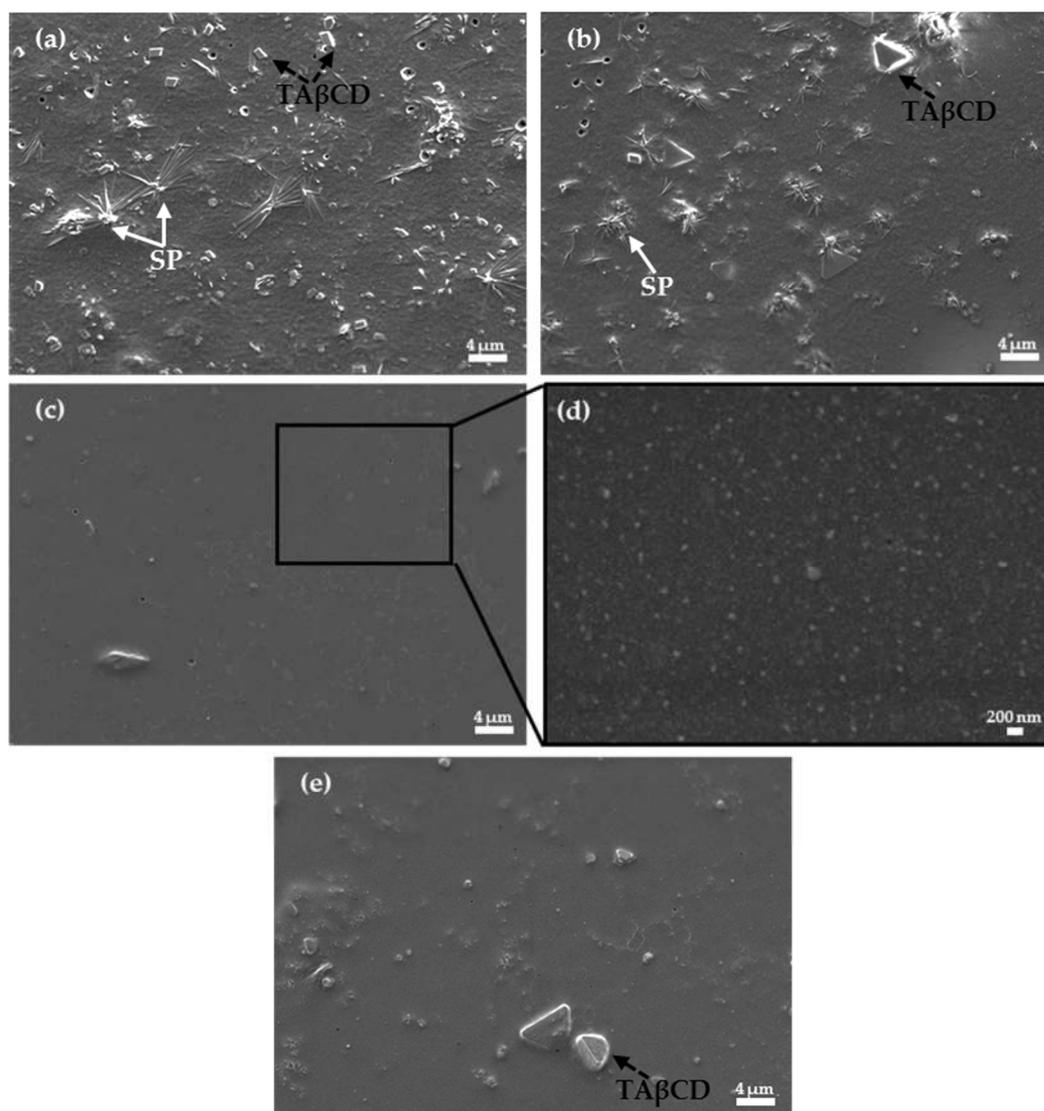
292 Where  $SP_{\text{nanoparticle}}$  is the weight of SP in the nanoparticles and  $NP_t$  is the total weight of nanoparticles  
 293 used for the quantification.

294 SP is hydrophilic and thus, its water-soluble nature makes it of difficult physical loading within  
 295 hydrophobic mPEG-PCL nanoparticles, resulting in %EE and DL of 9-14% and 0.2-0.6% (**Table**  
 296 **4**). Similar or lower values were obtained with DWC systems. These results were consistent with DLS  
 297 data, confirming that in this method, there is no effective entrapment of SP molecules within the PCL  
 298 domains of the nanoparticle regardless of the presence of TAβCD molecules. When the CD was used  
 299 to hydrophobize SP by spray-drying, both %EE and DL increased. In this context, the highest %EE  
 300 and DL values (85% and 2.6%, respectively) were observed for SP-loaded nanoparticles produced  
 301 with SP1/TAβCD1 SD and 2 mg of SP in the nanoprecipitation.

#### 302 2.3.5. Morphological characterization of SP-loaded nanoparticles.

303 Representative SP-loaded nanoparticles were visualized using HR-SEM (**Figure 6**). For this,  
 304 nanoparticles suspensions were drop-casted on silicon wafer. Upon water evaporation and drying of  
 305 the sample, free SP crystallizes and forms needle-like crystals, similar to those observed during TEM  
 306 analysis (**Figure 4b**). Free TAβCD can also undergo crystallization upon drying and form well-  
 307 defined prismatic crystals or, conversely, to remain amorphous and form glassy chips [31]. As it can

308 be seen, in SP-loaded nanoparticles prepared by the DWC method using 1 and 2 mg equivalent  
309 amounts of SP (**Figure 6a,b**, respectively), both SP and TA $\beta$ CD crystals were observed, confirming  
310 the presence of free SP and TA $\beta$ CD in the nanoparticle suspension. As for SP-loading nanoparticles  
311 prepared using spray-dried complexes, in case of TA $\beta$ CD1-SP1 with 1 mg of SP, there were no SP or  
312 TA $\beta$ CD crystals (**Figure 6c,d**). However, TA $\beta$ CD2-SP1 produced with 1 mg of SP, several glassy  
313 TA $\beta$ CD chips were seen. These findings indicated that a higher relative weight fraction of TA $\beta$ CD  
314 used in the production of the complex with SP resulted in an excess of TA $\beta$ CD which was not  
315 efficiently entrapped within the PCL matrix of the nanoparticle formed during the nanoprecipitation.  
316 In other words, the excess of TA $\beta$ CD precluded the formation of stable mPEG-PCL nanoparticles.  
317 Overall these observations were in a good agreement with DLS data and confirmed that additional  
318 size populations observed in DLS analysis were associated with the presence of free or aggregated  
319 TA $\beta$ CD.  
320



321

322 **Figure 6.** HR-SEM micrographs of SP-loaded mPEG-PCL nanoparticles utilizing (a) SP1/ TA $\beta$ CD1  
323 DWC (1 mg of SP), (b) SP1/TA $\beta$ CD1 DWC (2 mg of SP), (c) encapsulation of spray-dried SP1/TA $\beta$ CD1  
324 complex (1 mg of SP) under x5K, (d) x50K magnification of (c) and (e) and encapsulation of spray-  
325 dried SP1/TA $\beta$ CD2 complex (1 mg of SP).

326

## 327 4. Materials and Methods

### 328 4.1. Preparation of spray-dried TA $\beta$ CD-SP complexes.

329 TA $\beta$ CD (85 or 170 mg for 1:1 and 1:2 SP/TA $\beta$ CD complexes respectively; Sigma-Aldrich, St.  
330 Louis, MO, USA;) was dissolved in ethanol (19 and 38 mL for 1:1 and 1:2 complexes, respectively;  
331 Gadot, Netanya, Israel) with assistance of sonication in an ultrasonic bath (5 min, Elmasonic S 30,  
332 Elma Schmidbauer GmbH, Singen, Germany). SP (10 mg; Schricks Laboratories, Bauma, Switzerland)  
333 was dissolved in ethanol (12 mL) and mixed with the TA $\beta$ CD ethanol solution. The resulting binary  
334 solution was stirred under heating at 55°C (10 min; Hei-Tec Magnetic Stirrer, Heidolph Instruments,  
335 Schwabach, Germany) in order to prevent TA $\beta$ CD precipitation and subsequently spray-dried (Nano  
336 Spray Dryer B-90, Büchi Labortechnik AG, Flawil, Switzerland) using a closed loop configuration,  
337 under the following conditions: nitrogen flow 20 mL min<sup>-1</sup>, an inlet temperature of 55°C, an outlet  
338 temperature of 60°C and 80% spraying. The obtained powder was kept in a sealed vial at 4°C and  
339 protected from light until use.

340 Pure TA $\beta$ CD was spray-dried using the same method and named as processed TA $\beta$ CD. A SP  
341 reference sample (processed SP) was also prepared by dissolution of SP (10 mg) in ethanol (12 mL)  
342 and drying under vacuum (Vacuum Oven Lab-Line Instruments Inc., Dubuque, IL, US); SP is thermo-  
343 sensitive and undergoes degradation.

### 344 4.2. Preparation of PMs

345 PMs of SP and TA $\beta$ CD were prepared by mixing the pristine substances (1 mg of SP with 8.5 or  
346 17 mg of TA $\beta$ CD for 1:1 and 1:2 SP/TA $\beta$ CD PM, respectively) using a geometric dilution method by  
347 continually grinding substances in a mortar and pestle.

### 348 4.3. Characterization of spray-dried SP/TA $\beta$ CD complexes

349 Spray-dried SP/TA $\beta$ CD complexes (SD SP/TA $\beta$ CD) were fully characterized in order to confirm  
350 the formation of the complex and not of a PM.

#### 351 4.3.1. Differential scanning calorimetry

352 DSC analysis was performed in a DSC 2 STAR<sup>e</sup> system simultaneous thermal analyzer with  
353 STAR<sup>e</sup> software V13 (Mettler-Toledo, Schwerzenbach, Switzerland) at a heating rate of 10°C min<sup>-1</sup> in  
354 the 25–300°C temperature range under nitrogen flow of 20 mL min<sup>-1</sup> and using In as standard.

#### 355 4.3.2. Fourier-transform infrared spectroscopy

356 FTIR was recorded in an Equinox 55 spectrometer (Bruker Optics Inc., Ettlingen, Germany). Each  
357 sample (0.3% w/w) was thoroughly grinded with powdered KBr (Merck Chemical GmbH,  
358 Darmstadt, Germany) and compressed to a pellet under pressure of 10 MPa before the analysis.  
359 Spectra were obtained in the wavenumber range of 4000–500 cm<sup>-1</sup> with a resolution of 4 cm<sup>-1</sup> and 32  
360 scans were performed for each spectrum.

#### 361 4.3.3. Scanning electron microscopy

362 The surface morphology of the pure components and their binary combinations was visualized  
363 by HR-SEM (Zeiss Ultra-Plus FEG-SEM, Zeiss, Berkin, Germany), equipped with a high-resolution  
364 field emission gun. Samples were carbon sputtered prior to observation. The acceleration voltage was  
365 2–4 kV. Images were obtained using secondary electron detector at 3–4 mm working distance.

#### 366 4.3.4. Transmission electron microscopy

367 TEM was carried out in a Technai G2 T20 S-Twin (FEI, Eindhoven, Netherlands), operated at  
368 200 kV. Samples were dissolved in water, followed by placing three 10  $\mu$ L drops one after the other

369 on a carbon grid (Formvar/Carbon 300 mesh; Electron Microscopy Sciences, Hatfield, PA, USA).  
370 Samples were finally dried in a fume hood overnight before analysis.

#### 371 4.4. Preparation of SP-loaded mPEG-PCL nanoparticles

##### 372 4.4.1. Synthesis of mPEG-PCL copolymer

373 A mPEG-PCL block copolymer was synthesized by a solvent-free melt ROP of CL (5 g; Sigma-  
374 Aldrich) initiated by the terminal hydroxyl group of mPEG of molecular weight 4000 g mol<sup>-1</sup> (0.5 g;  
375 Tokyo Chemical Industry Co. Ltd. Tokyo, Japan). The polymerization was catalyzed by SnOct (142  
376 μL, 1:200 molar ratio to CL, Sigma-Aldrich) and carried out at 145°C (2.5 h) under nitrogen  
377 atmosphere (**Figure S1**). After the reaction, the crude mixture was cooled down to room temperature,  
378 dissolved in dichloromethane (Gadot) and precipitated in an excess of diethyl ether (Bio-Lab Ltd.,  
379 Jerusalem, Israel). The precipitated mPEG-PCL copolymer was filtered to remove remaining  
380 unreacted reagents, washed several times with diethyl ether, vacuum-dried at room temperature  
381 until constant weight and stored at -24°C until use. The formation of the copolymer was determined  
382 by <sup>1</sup>H-NMR at 400 MHz utilizing a Bruker Avance III High Resolution spectrometer (Bruker BioSpin  
383 GmbH, Rheinstetten, Germany). The M<sub>n</sub>, M<sub>w</sub> and Đ (M<sub>w</sub>/M<sub>n</sub>) of the copolymer were determined by  
384 GPC (Alliance HPLC System, Waters Corp., Milford, MA, USA) with refractive index detector and 4  
385 Styragel® HR (1-4) columns (7.8 X 300 mm, packed with 5 μm particles, Waters Corp.). The sample  
386 was prepared by dissolving mPEG-PCL copolymer (1% w/v) in tetrahydrofuran (THF, HPLC grade,  
387 Bio-Lab) and injecting 20 μL and the runs were conducted with a mobile phase flow of 1 mL min<sup>-1</sup>, at  
388 40°C. Poly(methyl methacrylate) standards (PSS polymer standards service, Mainz, Germany) with  
389 molecular weights between 2,260-171,000 g mol<sup>-1</sup> were used for molecular weights calibration.

##### 390 4.4.2. Drying of SP and TAβCD with mPEG-PCL copolymer

391 SP, TAβCD and mPEG-PCL, were dissolved in an acetone:methanol mixture (1:5 volume ratio)  
392 and magnetically stirred for 1 h at room temperature. Then, solvents were evaporated in a rotary  
393 evaporator (Rotavapor® R-100, Büchi Labortechnik AG) at room temperature and the dry solid  
394 mixture of SP, TAβCD and mPEG-PCL, was re-dissolved in anhydrous acetone. Nanoprecipitation  
395 was performed as described below.

##### 396 4.4.3. Encapsulation of free SP and SD SP/TAβCD complexes in mPEG-PCL nanoparticles by 397 nanoprecipitation

398 The encapsulation of pure SP and SD SP/TAβCD complexes in mPEG-PCL nanoparticles was  
399 performed using the nanoprecipitation method. In brief, the mPEG-PCL copolymer and SD  
400 SP/TAβCD complex (or pure SP) were dissolved in anhydrous acetone (10 mL) and the tertiary  
401 copolymer solution was added dropwise to degassed deionized distilled water (50 mL) in a sealed  
402 round-bottom flask under nitrogen flow to prevent the oxidation of SP due to exposure to air using  
403 a syringe pump (Laboratory Syringe Pump SYP-01, MRC Laboratory Equipment Manufacturer, Kfar  
404 Saba, Israel) at an injection rate of 0.333 mL min<sup>-1</sup> and under magnetic stirring (480 rpm, Hei-Tec  
405 Magnetic Stirrer). Then, the acetone was evaporated using a rotary evaporator (Rotavapor® R-100),  
406 at room temperature. The nanoparticle suspension was kept in a sealed vial at 4°C and protected  
407 from light until use. The production of SP-free mPEG-PCL nanoparticles was carried out using the  
408 same method, though without the addition of SP and the CD.  
409

#### 410 4.5. Characterization of SP-loaded nanoparticles

##### 411 4.5.1. Size and size distribution

412  $D_h$  and PDI of the different nanoparticles were measured by means of DLS (Zetasizer  
413 Nanoseries ZS90, Malvern Instruments, Malvern, UK).

414

##### 415 4.5.2. SP encapsulation efficiency and drug loading

416 For quantification of %EE and DL and, free SP was separated from the nanoparticles by  
417 ultrafiltration in Amicon® Ultra 15 mL Filters (MWCO 100 kDa, Merck Chemicals GmbH.). For this,  
418 each sample was centrifuged at 4500×g for 15 min at room temperature and SP was quantified in the  
419 filtrate fraction in a plate reader (Multiskan GO Microplate Spectrophotometer with SkanIt™  
420 software, Thermo Fisher Scientific Oy, Vantaa, Finland) employing a calibration curve of SP in water  
421 built in a range between 10 and 100  $\mu\text{g ml}^{-1}$  ( $R^2 = 0.996$ ).

##### 422 4.5.3. Morphological analysis of SP-loaded nanoparticles

423 Representative samples of SP-loaded nanoparticles were visualized by HR-SEM (Zeiss Ultra-  
424 Plus FEG-SEM). Samples were prepared by drop casting of 0.1% w/v nanoparticle suspension on a  
425 silicon wafer (CZ polished silicon wafers; SEH Europe Ltd., West Lothian, U.K.). Samples were  
426 carbon sputtered prior to analysis. The acceleration voltage was 2–4 kV. Images were obtained using  
427 secondary electron detector at 3–4 mm working distance.

428

429 **Supplementary Materials:** The following are available online at [www.mdpi.com/xxx/s1](http://www.mdpi.com/xxx/s1)

430 Figure S1. Chemical structure of BH4.

431 Figure S2. UV-Vis spectra of (a) pure BH4 and (b) pure SP solutions in water (1% w/v) at different  
432 times.

433 Figure S3: Ring opening polymerization of CL initiated by the hydroxyl groups of mPEG with  
434 molecular weight of 4000  $\text{g mol}^{-1}$ .

435 Figure S34  $^1\text{H-NMR}$  spectrum of the mPEG-PCL copolymer in  $\text{CDCl}_3$ .

436 Table S1: The number average molecular weight ( $M_n$ ), the weight average molecular weight ( $M_w$ ) and  
437 the dispersity ( $\text{Đ}$ ,  $M_w/M_n$ ), as determined by  $^1\text{H-NMR}$  and GPC.

438

439 **Funding:** This work was supported by the Niedersächsisches Ministerium für Wissenschaft und Kultur &  
440 VolkswagenStiftung (Grant #88681). Partial support of the Russell Berrie Nanotechnology Institute (RBNI,  
441 Technion) is acknowledged.

442

443 **Conflicts of Interest:** The authors declare no conflict of interest

444

#### 445 References

- 446 1. Thöny, B.; Auerbach, G.; Blau, N. Tetrahydrobiopterin biosynthesis, regeneration and  
447 functions. *Biochem. J.* **2000**, *347 Pt 1*, 1–16.
- 448 2. Thöny, B. Tetrahydrobiopterin and its functions. **2004**, 495–546.
- 449 3. Alp, N.J.; Channon, K.M. Regulation of Endothelial Nitric Oxide Synthase by  
450 Tetrahydrobiopterin in Vascular Disease. *Arterioscler. Thromb. Vasc. Biol.* **2004**, *24*, 413–420.
- 451 4. Hyland, K. Inherited Disorders Affecting Dopamine and Serotonin: Critical  
452 Neurotransmitters Derived from Aromatic Amino Acids. *J. Nutr.* **2007**, *137*, 1568S–1572S.
- 453 5. Blau, N.; Thöny, B.; Cotton, R.G.H.; Hyland, K. Disorders of tetrahydrobiopterin and related  
454 biogenic amines. In *The metabolic and molecular bases of inherited disease*; 2001; Vol. 2, pp. 1725–  
455 1776 ISBN 0079130356.
- 456 6. Davis, M.D.; Kaufm, S.; Milstein, S. The auto-oxidation of tetrahydrobiopterin. *Eur. J. Biochem.*

- 457           1988, 173, 345–351.
- 458   7.    Sosnik, A.; Carcaboso, A.; Chiappetta, D. Polymeric Nanocarriers: New Endeavors for the  
459    Optimization of the Technological Aspects of Drugs. *Recent Patents Biomed. Eng.* **2010**, *1*, 43–  
460    59.
- 461   8.    Moretton, M.A.; Glisoni, R.J.; Chiappetta, D.A.; Sosnik, A. Biointerfaces Molecular  
462    implications in the nanoencapsulation of the anti-tuberculosis drug rifampicin within flower-  
463    like polymeric micelles. *Colloids Surfaces B Biointerfaces* **2010**, *79*, 467–479.
- 464   9.    Maitz, M.F. Applications of synthetic polymers in clinical medicine. *Biosurface and Biotribology*  
465    **2015**, *1*, 161–176.
- 466   10.   Guo, J.; Gao, X.; Su, L.; Xia, H.; Gu, G.; Pang, Z.; Jiang, X.; Yao, L.; Chen, J.; Chen, H. Aptamer-  
467    functionalized PEG–PLGA nanoparticles for enhanced anti-glioma drug delivery. *Biomaterials*  
468    **2011**, *32*, 8010–8020.
- 469   11.   Danafar, H.; Davaran, S.; Rostamizadeh, K.; Valizadeh, H.; Hamidi, M. Biodegradable m-  
470    PEG/PCL core-shell micelles: Preparation and characterization as a sustained release  
471    formulation for curcumin. *Adv. Pharm. Bull.* **2014**, *4*, 501–510.
- 472   12.   Peng, W.; Jiang, X.; Zhu, Y.; Deng, W.; Yu, J.; Xu, X.; Zhang, W. Oral delivery of capsaicin  
473    using MPEG-PCL nanoparticles. *Acta Pharmacol. Sin.* **2014**, *36*, 139–148.
- 474   13.   Riley, T.; Govender, T.; Stolnik, S.; Xiong, C.D.; Garnett, M.C.; Illum, L.; Davis, S.S. Colloidal  
475    stability and drug incorporation aspects of micellar-like PLA- PEG nanoparticles. *Colloids*  
476    *Surfaces B Biointerfaces* **1999**, *16*, 147–159.
- 477   14.   Danafar, H. MPEG–PCL copolymeric nanoparticles in drug delivery systems. *Cogent Med.*  
478    **2016**, *3*, 1142411.
- 479   15.   Grossen, P.; Witzigmann, D.; Sieber, S.; Huwyler, J. PEG-PCL-based nanomedicines: A  
480    biodegradable drug delivery system and its application. *J. Control. Release* **2017**, *260*, 46–60.
- 481   16.   Pannirselvam, M.; Simon, V.; Verma, S.; Anderson, T.; Triggler, C.R. Chronic oral  
482    supplementation with sepiapterin prevents endothelial dysfunction and oxidative stress in  
483    small mesenteric arteries from diabetic (db/db) mice. *Br. J. Pharmacol.* **2003**, *140*, 701–706.
- 484   17.   Massella, D.; Celasco, E.; Salaün, F.; Ferri, A.; Barresi, A.A. Overcoming the limits of flash  
485    nanoprecipitation: Effective loading of hydrophilic drug into polymeric nanoparticles with  
486    controlled structure. *Polymers (Basel)*. **2018**, *10*.
- 487   18.   Barichello, J.M.; Morishita, M.; Takayama, K.; Nagai, T. Encapsulation of Hydrophilic and  
488    Lipophilic Drugs in PLGA Nanoparticles by the Nanoprecipitation Method. *Drug Dev. Ind.*  
489    *Pharm.* **1999**, *25*, 471–476.
- 490   19.   Londhe, A.S. and V. Inclusion Complexes of Hydroxy Propyl-beta-Cyclodextrin and  
491    Paliperidone: Preparation and Characterization. *Curr. Drug Discov. Technol.* **2014**, *11*, 271–278.
- 492   20.   Yang, H.; Parniak, M.A.; Isaacs, C.E.; Hillier, S.L.; Rohan, L.C. Characterization of cyclodextrin  
493    inclusion complexes of the anti-HIV non-nucleoside reverse transcriptase inhibitor UC781.  
494    *AAPS J.* **2008**, *10*, 606–613.
- 495   21.   Loftsson, T.; Ólafsdóttir, B.J.; Friðriksdóttir, H.; Jónsdóttir, S. Cyclodextrin complexation of  
496    NSAIDs: physicochemical characteristics. *Eur. J. Pharm. Sci.* **1993**, *1*, 95–101.
- 497   22.   Loftsson, T.; Hreinsdóttir, D.; Másson, M. Evaluation of cyclodextrin solubilization of drugs.  
498    *Int. J. Pharm.* **2005**, *302*, 18–28.
- 499   23.   Nakanishi, K.; Masukawa, T.; Nadai, T.; Yoshii, K.; Okada, S.; Miyajima, K. Sustained release

- 500 of flufenamic acid from a drug-triacetyl-beta-cyclodextrin complex. *Biol. Pharm. Bull.* **1997**, *20*,  
501 66–70.
- 502 24. Fernandes, C.M.; Veiga, F.J.B. Effect of the hydrophobic nature of triacetyl-beta-cyclodextrin  
503 on the complexation with nifedipine hydrochloride: physicochemical and dissolution  
504 properties of the kneaded and spray-dried complexes. *Chem. Pharm. Bull. (Tokyo)*. **2002**, *50*,  
505 1597–1602.
- 506 25. Fernandes, C.M.; Ramos, P.; Jose, F. Hydrophilic and hydrophobic cyclodextrins in a new  
507 sustained release oral formulation of nifedipine: in vitro evaluation and bioavailability  
508 studies in rabbits. **2003**, *88*, 127–134.
- 509 26. Corti, G.; Capasso, G.; Maestrelli, F.; Cirri, M.; Mura, P. Physical – chemical characterization  
510 of binary systems of metformin hydrochloride with triacetyl- $\beta$ -cyclodextrin. **2007**, *45*, 480–  
511 486.
- 512 27. Nunes, A.V.M.; Almeida, A.P.C.; Marques, S.R.; Sousa, A.R.S. De; Casimiro, T.; Duarte,  
513 C.M.M. Processing triacetyl- $\beta$ -cyclodextrin in the liquid phase using supercritical CO<sub>2</sub>. *J.*  
514 *Supercrit. Fluids* **2010**, *54*, 357–361.
- 515 28. Bratu, I.; Veiga, F.; Fernandes, C.; Hernanz, A.; Gavira, J.M. Infrared spectroscopic study of  
516 triacetyl- $\beta$ -cyclodextrin and its inclusion complex with nifedipine. *Spectroscopy* **2004**, *18*, 459–  
517 467.
- 518 29. Ghorab, M.K.; Adeyeye, M.C. Enhancement of Ibuprofen Dissolution via Wet Granulation  
519 with  $\beta$ -Cyclodextrin. *Pharm. Dev. Technol.* **2001**, *6*, 305–314.
- 520 30. Carneiro, S.B.; Duarte, F.Í.C.; Heimfarth, L.; Quintans, J.D.S.S.; Quintans-Júnior, L.J.; Júnior,  
521 V.F.D.V.; De Lima, Á.A.N. Cyclodextrin-drug inclusion complexes: In vivo and in vitro  
522 approaches. *Int. J. Mol. Sci.* **2019**, *20*, 1–23.
- 523 31. Bettinetti, G.; Sorrenti, M.; Catenacci, L.; Ferrari, F.; Rossi, S. Polymorphism,  
524 pseudopolymorphism, and amorphism of peracetylated  $\alpha$ -,  $\beta$ -, and  $\gamma$ -cyclodextrins. *J. Pharm.*  
525 *Biomed. Anal.* **2006**, *41*, 1205–1211.
- 526 32. Sami, F.; Philip, B.; Pathak, K. Effect of auxiliary substances on complexation efficiency and  
527 intrinsic dissolution rate of gemfibrozil-beta-CD complexes. *AAPS PharmSciTech* **2009**, *11*, 27–  
528 35.
- 529 33. Dollo, G.; Le Corre, P.; Chollet, M.; Chevanne, F.; Bertault, M.; Burgot, J.L.; Le Verge, R.  
530 Improvement in solubility and dissolution rate of 1,2-dithiole-3-thiones upon complexation  
531 with  $\beta$ -cyclodextrin and its hydroxypropyl and sulfobutyl ether-7 derivatives. *J. Pharm. Sci.*  
532 **1999**, *88*, 889–895.
- 533 34. Sapte, S.; Pore, Y. Inclusion complexes of cefuroxime axetil with  $\beta$ -cyclodextrin:  
534 Physicochemical characterization, molecular modeling and effect of l-arginine on  
535 complexation. *J. Pharm. Anal.* **2016**, *6*, 300–306.  
536