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Hydration and Fat Estimates

[Gian Luca Farina](#)*, Carmine Orlandi, Niccolò Gori, [Lexa Nescolarde](#), [Henry Lukaski](#)

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Articles

Fluid Imbalance Clarifies Bioelectrical Impedance Analysis Fat Estimates Discrepancies, Dual-Energy X-ray Absorptiometry

Gian Luca Farina ¹, Carmine Orlandi ², Niccolò Gori ³, Lexa Nescolarde ⁴ and Henry Lukaski ⁵

¹ Medical Center Eubion, 00135 Rome, Italy; gianluca.farina@biologo.onb.it

² Medical Center Eubion, Tor Vergata University, Medical Faculty, 00133 Rome, Italy; carmine.orlandi@uniroma2.it

³ Federazione Italiana Rugby-FIR, Stadio Olimpico, Foro Italico, 00135 Rome, Italy; niccolo.gori@federugby.it

⁴ Department of Electronic Engineering, Universitat Politècnica de Catalunya, 08034 Barcelona, Spain; lexa.nescolarde@upc.edu

⁵ Department of Kinesiology and Public Health Education, University of North Dakota, Grand Forks, 58201 North Dakota, USA; henry.lukaski@und.edu⁴

* Correspondence: gianluca.farina@biologo.onb.it

Abstract: Limitations of body mass index (BMI) as a measure of body fat and the need for practical methods to estimate body fat increase interest in smartphone two-dimensional digital imaging and bioelectrical impedance analysis (BIA). Compared to dual x-ray absorptiometry (DXA), we determined differences in body fat mass (FM) analysis (BIA) in 188 healthy adults (69 females and 119 males). BIA underestimated ($p < 0.0001$) FM. We tested the hypothesis that fluid imbalance, expansion of the extracellular water (ECW), designated as ECW to intracellular ratio (ECW/ICW), affects the BIA-dependent differences. With $BMI > 25$ kg/m², 54 male rugby players, compared to 40 male non-rugby players, had greater ($p < 0.001$) BMI and fat-free mass but less ($p < 0.001$) FM and ECW/ICW. BIA underestimated ($p < 0.001$) FM in the non-rugby men. This finding is consistent with expansion of ECW in individuals with excess body fat due to increased adipose tissue mass and its water content. BIA predictions of FM are affected by altered fluid distribution associated with increased adipose tissue.

Keywords: smartphone; fat; extracellular water; body mass index; digital imaging; bioelectrical impedance

1. Introduction

Obesity is a multifactorial chronic disease that increases the risk of long-term morbidity, reduces life span, and increases health care costs. More than 650 million people worldwide were identified as obese in 2016 representing a three-fold increase since 1975 [1]. Four million deaths in 2015 were attributed to obesity, and two-thirds ascribed to cardiovascular disease [2]. The global economic burden of obesity is expected to be USD 1.2 trillion in 2025 [3]. Thus, the availability of reliable and practical methods to identify individuals with excess body fat is a public health need.

Clinicians and health professionals use ranges of body weight relative to height, body mass index (BMI; Wt/Ht^2), to stratify adiposity-related health risks in a population. The convenience of BMI in clinical and research settings is offset by its unreliability to estimate body fat and predict the risk of obesity-related diseases for an individual [3–10]. Because BMI is an insensitive indicator of body composition, it poorly predicts the adiposity of individuals with increased fat-free mass (FFM) [11,12]. Other methods to estimate body composition improve the specificity and precision of estimation of fat and lean body components but are limited by technical complexity, exposure to ionizing radiation, invasiveness, lack of mobility, and cost that prevent their widespread use for routine assessment of body composition [13,14]. Recent reports describe the limitations of BMI and emphasize the need for practical and valid methods to identify overweight and obesity and thus improve the care of patients with excess body fat [15–17].

Two methods are amenable to meet this clinical need. Bioelectrical impedance analysis (BIA) relies on the conduction of a safe, administered alternating current to estimate total body water (TBW) [18]. Most BIA methods use 50 kHz phase-sensitive devices and rely on the assumption of constant hydration to estimate FFM and calculate body fat. Alternatively, smartphone two-dimensional standing digital image analysis (2DI) coupled with computational machine learning has recently been used to estimate total body adiposity [19–22]. Studies reported differences in body fat estimates using smartphone 2DI and BIA compared to DXA but have not provided explanations for the observations [20,21]. Whereas BIA is a valid method to assess TBW [18] and excess body fat increases ECW [23], reliance on the assumption of constant hydration of the FFM may overestimate FFM and, thus, underestimate body fat in adults who are overweight or obese [24,25]. We hypothesize that fluid imbalance is a factor explaining differences in fat estimation with BIA compared to digital imaging.

The aim of the present study was to compare body fat mass (FM) estimates derived using BIA relative to dual x-ray absorptiometry (DXA) in healthy adults and to determine whether fluid imbalance contributes to any observed differences in FM estimates.

2. Materials and Methods

2.1. Participants

We recruited healthy adult Caucasian women and men aged 19 to 64 y using advertisements and word of mouth to participate in this study, which was conducted at the Eubion Medical Center and Tor Vergata University, in Rome, Italy. Prospective participants underwent a clinical examination and completed a health questionnaire to establish the absence of an unhealthy condition prior to participation. Exclusion criteria include metal implants, current treatment for metastatic disease, diabetes, diuretic therapy, or limb loss. This study was conducted in accordance with the Declaration of Helsinki and approved by the Institutional Review Board of the University of Tor Vergata. Each participant provided written informed consent prior to participation in any testing.

2.2. Body composition assessment

Volunteers, wearing form-fitting clothing without jewelry, came to the laboratory after consuming a light meal and emptying their bladders. Standing height and body weight were determined using standard medical equipment (SECA Stadiometer and SECA 762 scale; Hamburg, Germany).

Body composition estimation included BIA, and DXA administered in random order. Volunteers underwent whole-body BIA testing using a 50 kHz phase-sensitive impedance analyzer that introduced a sinusoidal, constant current (250 μ A RMS) (BIVA, EFG 3 Monitor; Akern, Florence, Italy) using a tetrapolar surface electrode placement with paired current-injecting and voltage drop-measuring electrodes (BIAtrodes; Akern, Florence, Italy) separated a minimum of 5 cm and placed on the right wrist and ankle. Volunteers rested supine on a bed without contact with metal for 10 min. This BIA instrument provided direct measurements of resistance (R), reactance (Xc), and phase angle (PhA). The technical accuracy and precision of the BIA instrument were determined with a calibrated precision parallel circuit formed by a 384 Ω (\pm 1%) resistor in parallel with a 780 pF (\pm 2%) capacitor yielding 47 Ω of Xc at 50 kHz.

Body composition was estimated by using the following BI prediction models. Kyle et al. [26] (BIA1):

FFM = 4.104 + 0.518 Ht²/R + 0.231 Wt + 0.130 Xc + 4.229 Sex* [1 for men and 0 for women] Sun et al. [27] (BIA2):

Males: FFM = -9.88 + 0.65 Ht²/R + 0.26 Wt + 0.02 R

Females: FFM = -11.03 + 0.70 Ht²/R + 0.07 Wt + 0.02 R

Units are FFM (kg), height (Ht)²/R (cm²/ Ω), weight (Wt, kg), and Xc (Ω).

We also estimated body composition using the proprietary equations of the BIA instrument manufacturer (Bodygram PLUS; Akern, Florence, Italy) (BIA3). This approach estimates the actual hydration (water content) of the FFM of an individual and uses the measured hydration in lieu of the

customary 0.732 steady-state hydration ratio to estimate FFM (Akern BodyGram PRO; Florence, Italy). Fat mass is calculated as the difference between body weight and FFM.

Reference whole-body composition was determined using DXA, a GE Lunar iDXAncore sn 200278 using software version 14.10.022 (Madison, WI). All participants were positioned supine and scanned within the dimensions of the DXA table. Precision estimates were 1.3% for FM and 0.5% for FFM.

Fluid distribution was evaluated using BIA measurements and bioelectrical impedance vector analysis (BIVA) [28]. This method uses tetrapolar BIA and a 50 kHz phase-sensitive impedance device and provides whole-body, direct serial measurements of resistance (R), reactance (Xc), and phase angle (PhA). One measure was the ratio of ECW to total body water (TBW), ECW%, which was estimated with a proprietary model (Akern BodyGram PLUS; Florence, Italy). We also assessed fluid distribution (ECW/ICW) using PhA, which is inversely related to ECW/ICW [29].

2.3. Statistical Methods

Statistical analyses were performed using SYSTAT version 13 (Systat Corporation; San Jose, CA, USA) and version 19.0.3 (MedCalc Software Bvba, Ostend, Belgium). Descriptive data are expressed as mean \pm SD. Statistical significance was set at $p < 0.05$.

Estimates of FM for each BIA prediction model were compared with the reference DXA values. Measurement agreement was evaluated with concordance correlation coefficient (CCC) [29], standard error of the estimate (SEE) between DXA and each method. Reference and estimates of body fat values in each sex group were compared separately with a paired t-test. Bland–Altman plot [30,31] was used to determine bias and limits of agreement (LOA) for BIA methods compared to DXA determinations.

Effects of fluid distribution were evaluated in a sub-group of males with BMI greater than 25 kg/m², the population indicator for overweight and obesity to contrast the effects of differences in adipose tissue with an unpaired t-test. Differences between group vector distributions were determined using Hotelling's T2 test.

3. Results

Table 1 describes the physical characteristics of the participants and shows the wide ranges of BMI and FM in the groups.

Table 1. Physical characteristics of the study participants. Values are mean \pm SD (min – max).

	Females	Males	Males BMI ^A >25 kg/m ²	
		Total	Rugby	Non-rugby
N	69	119	54	40
Height, cm	162.7 \pm 6.3 (150.0-178.0)	182.5 \pm 8.7 (160.0-202.0)	186.2 \pm 7.2 (173.0-202.0)	179.7 \pm 9.2 (163.0-198.0)
Weight, kg	67.8 \pm 14.5 (41.8-103.6)	93.2 \pm 13.3 (61.1-125.6)	104.8 \pm 11.4 (79.4-123.0)	91.4 \pm 12.2 (69.5-124.6)
BMI, kg/m ²	25.6 \pm 5.4 (16.1-37.2)	27.6 \pm 4.0 (19.5-37.0)	30.4 \pm 3.3 (25.2-36.6)	28.7 \pm 3.0 (25.1–37.1)
Fat mass ^B , kg	24.3 \pm 11.6 (6.4-52.3)	18.8 \pm 7.67 (5.6-35.2)	19.3 \pm 6.5 (9.0–35.2)	23.3 \pm 6.9 (10.3–35.1)
Fat ^B , %	34.2 \pm 10.2 (12.1-50.5)	19.8 \pm 6.7 (8.3-36.8)	18.2 \pm 4.7 (9.8- 28.9)	25.4 \pm 6.2 (11.4-36.8)
Fat-free mass ^B , kg	43.5 \pm 5.6 (31.0-55.8)	74.4 \pm 12.7 (47.4-103.2)	84.7 \pm 6.6 (68.9-103.2)	68.1 \pm 10.1 (50.6-97.2)

^A BMI: Body Mass Index; ^B Dual x-ray absorptiometry.

Levels of agreement differed between the reference and candidate methods (Table 2). All BIA equations underestimated ($p < 0.0001$) FM (1.1 \pm 2.4, 3.2 \pm 2.4, and 3.6 \pm 2.3 kg) in females. One BIA

model underestimated FM (2.4 ± 3.7 kg) and two BIA equations overestimated ($p < 0.0001$) FM (1.44 ± 3.9 and 2.9 ± 3.7 kg) in males.

Table 2. Levels of agreement (F and M) for body fat estimates using smartphone single lateral standing digital image analysis and 50 kHz bioelectrical impedance analysis compared to dual x-ray absorptiometry.

Group	Method	Fat mass, kg	Bias, kg	p	SEE, kg	CCC	MAE, kg	MAPE, %	LOA, kg
Females	DXA	24.3±11.6							
	BIA1	23.2±10.6	1.1±2.4	0,0001	2,3	0,98	2,2	8,9	5,8, -3,6
	BIA2	21.1±10.9	3.2±2.4	0,0001	2,3	0,94	3,4	13,6	7,8, -1,5
	BIA3	20.7±11.3	3.6±2.3	0,0001	2,3	0,93	3,6	15,1	8,1, -0,9
Males	DXA	18.8±7.6							
	BIA1	20.3±8.2	-1.4±3.9	0,0001	3,7	0,86	3,3	16,9	6,2, -9,1
	BIA2	21.1±7.3	-2.9±3.7	0,0001	3,6	0,84	3,6	19	9,5, -4,9
	BIA3	16.4±7.5	2.4±3.6	0,0001	3,6	0,84	3,6	18,1	9,6, -4,7

RMSE = root mean square; Bias = DXA - method; p=probability value; CCC = concordance correlation coefficient; MAE = mean absolute error; MAPE = mean absolute percent error; LOA = limits of agreement; BIA1 = Kyle et al. [26]; BIA2 = Sun et al. [27]; BIA3 = Akern (proprietary model) DXA = dual x-ray absorptiometry;

Figure 2 reveals differences. According to McBride [29], Among females, BIA1 showed substantial concordance (0.98) while BIA2 and BIA3 showed moderate concordance (0.94 to 0.93) with DXA. In contrast, all male samples showed poor CCC (< 0.90) between the BIA prediction models and DXA.

For females, BIA, had greater MAE in males (3.3 to 3.6 vs 2.3 kg). Mean absolute percent error (MAPE) BIA for females and males (8.6 vs 8.9 to 15% and 11.5 vs 16.9 to 19%, respectively).

The intercepts for the BIA2 and BIA3 (2.3 and 3.4 kg; $p < 0.0001$) prediction models in females and BIA1, BIA2, and BIA3 (2.16, 3.50 and 4.11 kg; $p < 0.0001$) in males were different from 0. The slopes for these lines were variable from 1.0 to 1.08 in females and from 0.82 to 0.99 for males, but not different than 1. The SEE in females (2.3 kg) was less than SEE in males (3.7 kg)

Compared to DXA, the BIA predictions of FM had significant bias in females (1.1 to 3.6 kg; $p < 0.0001$) and males (2.3 and 2.4 kg; $p < 0.0001$) with one BIA equation overestimating FM (-1.4 kg; $p < 0.0001$). The slopes of the lines relating the differences between DXA and individual methods were different ($p < 0.0001$) than 0 for two of the BIA equations in the females.

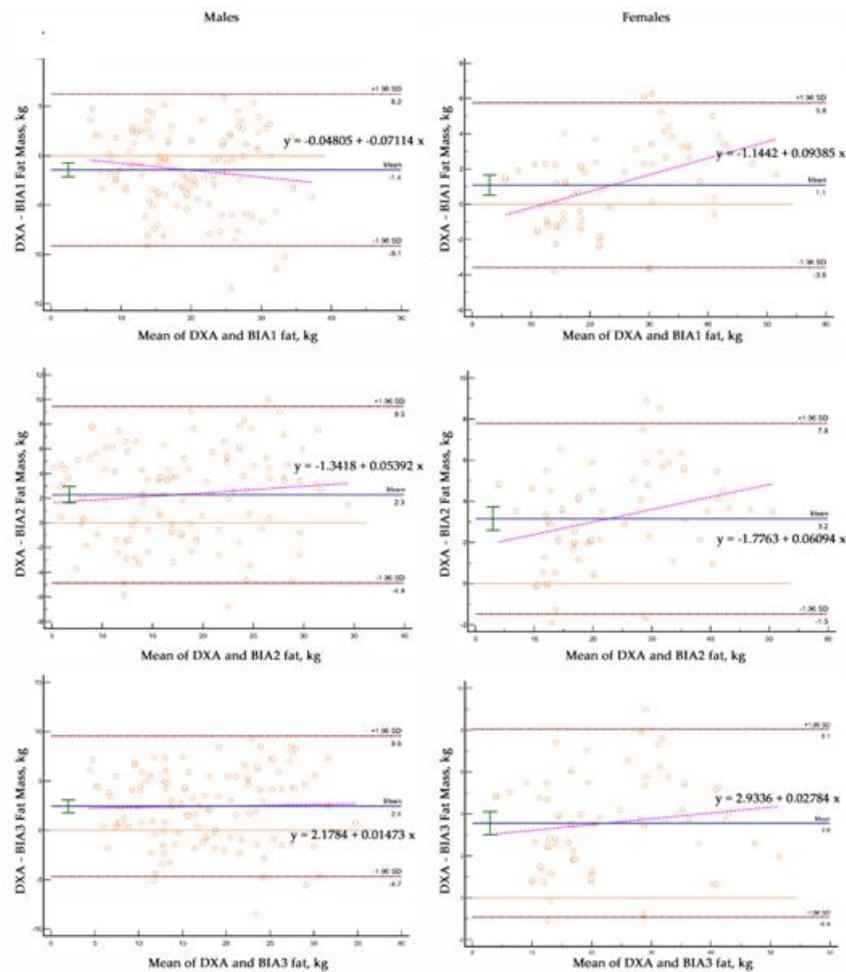


Figure 3. Bland-Altman plots Males and Females.

We tested the hypothesis that excess fat affected fluid balance in men with BMI > 25 kg/m² by comparing male elite male rugby players with men who were non-rugby players (Table 2). Compared to non-rugby men, male rugby players had greater BMI (30.04 ± 3.3 vs 28.7 ± 3.0 kg/m²; $p < 0.05$) and FFM (84.7 ± 6.6 vs 68.1 ± 10.1 kg; $p < 0.0001$) with less FM (19.3 ± 6.6 vs 23.3 ± 6.8 kg; $p < 0.01$), %fat (18.2 ± 4.7 vs $25.4 \pm 6.2\%$; $p < 0.0001$) and ECW% (36.2 ± 2.4 vs $39.54 \pm 3.5\%$; $p < 0.001$).

Compared to DXA, one BIA equation overestimated FM (4.1 ± 3.3 kg; $p < 0.0001$) in rugby players and two BIA models underestimated FM (3.7 ± 3.5 and 4.2 ± 3.6 kg; $p < 0.0001$) in non-rugby males. Concordance was poor for all BIA equations. For both groups, BIA, had a MAE (2.6 to 4.8 vs 2.6 kg and 2.7 to 34.3 vs 2.1 kg, respectively) and MAPE (11.3 to 21.4 vs 7.9% and 8.3 to 20.9 vs 10.8%, respectively).

Table 3. Levels of agreement R and Non-rugby for body fat estimates using smartphone single lateral standing digital image analysis and 50 kHz bioelectrical impedance analysis compared to dual x-ray absorptiometry of men with body mass index greater than 25 kg/m².

Group	Method	Fat mass, kg	Bias, kg	p	SEE, kg	CCC	MAE, kg	MAPE, %
Rugby	DXA	19.3±6.6						
	BIA1	23.4±6.8	4.0±3.3	0,0001	3,1	0,78	4,3	21,4
	BIA2	18.5±6.2	-0.9±3.6	0,08	3,5	0,85	3	14,3
	BIA3	18.8±6.4	-0.5±3.4	0,24	3,3	0,88	2,7	11,3
Non-rugby	DXA	23.3±6.8						
	BIA1	22.8±6.5	-0.5±3.4	0,36	3,4	0,87	2,6	8,3

BIA2	19.7±5.9	-3.7±3.5	0,0001	3,5	0,73	4,4	19,1
BIA3	19.1±6.1	-4.2±3.6	0,0001	3,4	0,72	4,8	20,9

RMSE = root mean square; Bias = DXA - method; p=probability value; CCC = concordance correlation coefficient; MAE = mean absolute error; MAPE = mean absolute percent error; LOA = limits of agreement; BIA1 = Kyle et al. [26]; BIA2 = Sun et al. [27]; BIA3 = Akern (proprietary model) DXA = dual x-ray absorptiometry;

Compared to DXA FM values, BIA predictions differed significantly from the line of identity (Figure 4).

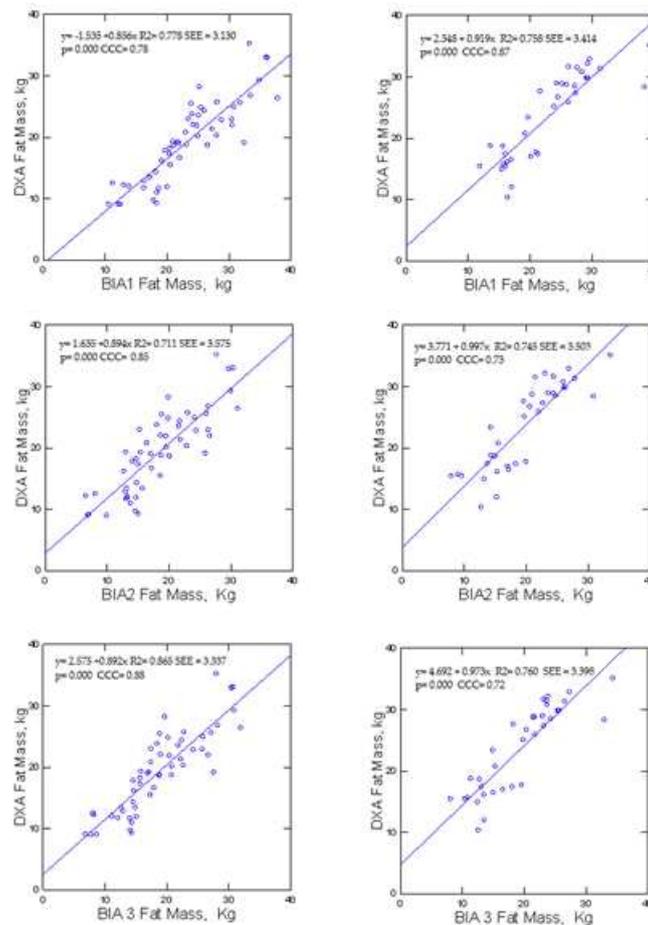


Figure 4. Linear regression Rugby (left) and Non-Rugby men (right).

Bland-Altman analysis revealed significant bias and greater variability of data with BIA equations (Figure 5 and Table 3). Fat mass was significantly overestimated (4.0 ± 3.3 kg) with one BIA equation in rugby players. One BIA equation underestimated FM (-0.9 ± 3.6 kg) in the rugby males and all BIA equations significantly underestimated FM in the non-rugby players (-3.7 ± 3.5 and -4.2 ± 3.6 kg). The slopes of the lines relating the differences between DXA and individual methods were different ($p < 0.0001$) than 0 for the BIA equations in all male groups.

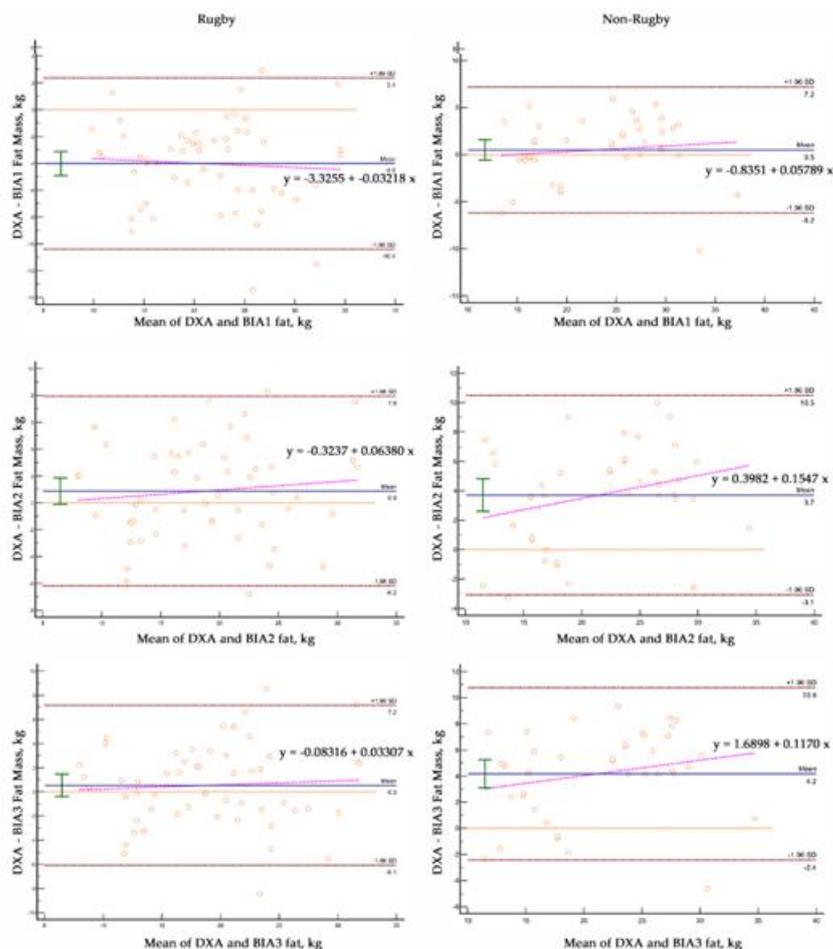


Figure 5. Bland-Altman plots Rugby and Non-Rugby.

Figure 6 shows the significant group differences ($p < 0.0001$) between the 95% confidence ellipses of men with BMI > 25 kg/m². The rugby players had a shorter impedance vector displaced to the left indicating greater conductive mass and structure than the non-rugby males. The larger PhA of the rugby players designates less relative ECW or ECW/ICW compared to the non-athletic men associated with the lesser FM.

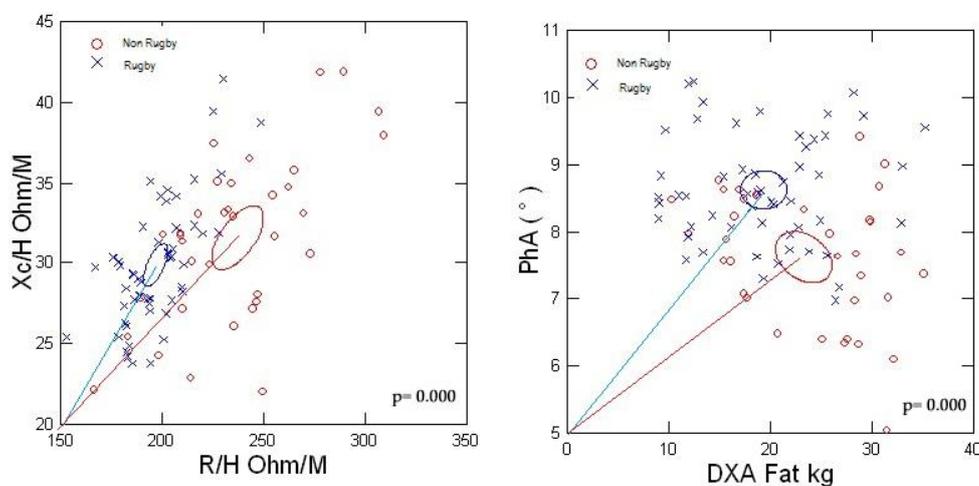


Figure 6. 95% confidence ellipses for R and NR AND PhA vs DXA FM for R and NR

4. Discussion

Awareness of the limitations of BMI coupled with interest by clinicians and public health researchers for point-of-contact methods to estimate body adiposity is growing [15–17]. Characteristics such as validity, high reproducibility, mobility, cost-effectiveness, and simplicity for operators focused research on BIA to meet this need. The findings of the present study demonstrate significant underestimation of FM with BIA. These results are consistent with other comparative studies of 2DI and BIA relative to reference DXA determinations of body fat [20,21]. However, they provide the first evidence that fluid imbalance contributes to the errors of BIA in estimating body fat.

A few reports speculated that increased body fat could adversely impact the validity of BIA predictions of FFM [24,25]. The researchers proposed that an expansion of ECW would contribute to an overestimation of FFM but provided no evidence. We evaluated this hypothesis in a subgroup of men with BMI > 25 kg/m² with different body composition profiles. Male rugby players, compared to non-rugby playing men, had decreased specific resistivity (R/Ht; 196.98±17.21 vs 237.22±30.97 ohm/m; p<0.0001) and increased FFM (84.7 vs 68.1 kg; p<0.001) with decreased FM (19.3 vs 23.3 kg; p<0.001) and ECW% (36.23±2.4 vs 39.54±3.5%; p<0.001). The decreased specific resistivity, or increased conductivity, reflects greater TBW and FFM in the rugby players. The increased ECW% among the non-rugby men indicates altered fluid distribution in association with the increased body fat and reduced ICW due to less FFM. Increased body fat is associated with an expanded adipose tissue volume that is directly related to an expanded ECW, absolute and relative, previously reported among adults classified as obese using BMI criteria [23,33]. Chemical analyses demonstrated the appreciable water content of adipose tissue as 15% [34], which contributes to its conductivity but to a lesser degree than muscle. Thus, inter-individual differences in body fat contribute to the variability of ECW in adults.

Raw BIA measurements provide additional support for the finding of increased ECW. The significantly decreased PhA values in the non-rugby men indicate an expansion of ECW based on tracer dilution determinations of fluid volumes and demonstrate an inverse relationship between PhA and ECW/ICW [32]. Also, a decreased PhA has been associated with an expansion of ECW in novice runners with increased risk of acute kidney injury after a marathon [35]. The findings of imbalanced fluid distribution, ECW/ICW, contribute to the concerns regarding the assumption of constant hydration inherent in the application of BIA to estimate FFM and predict body fat [36–38].

The independent variables in the BIA prediction models offer potential sources of error in the prediction of FFM. The common predictors of Ht²/R and R are significantly related to TBW. Thus, an increase of ECW in individuals with excess body fat increases TBW and decreases R, which assuming constant hydration of FFM, can overestimate FFM and thus underestimate FM. The BIA models also include body weight, which is highly correlated with body fat, and can vary depending on environmental, dietary, and physical activity conditions and hence affect hydration. Additionally, the application of BIA prediction equations in groups in whom the original model was not developed can lead to errors. It is well established that body geometry (e.g., limb length, cross-sectional area, and volume) and fluid content (total and distribution) directly affect resistivity and contribute to inter-individual differences in whole body and regional BIA measurements [36,39]. Additionally, regional BIA measurements using different electrode placements, such as foot-to-foot and hand-to-hand, yield discordant estimates of body composition compared to whole-body measurements [40]. These factors contribute to the errors in BIA predictions of body fat using various BIA methods and models and DXA in the present study and other reports [20,21].

This study has some limitations. The inference of expansion of ECW relies on qualitative assessments using BIA. Future studies should incorporate tracer dilution determinations of ECW and TBW and obtain threshold values at which altered fluid distribution affect errors in estimating body fat using BIA. Additionally, investigators should determine the effect of graded body fat levels on errors relative to criteria reference methods particularly in adults with sarcopenic obesity.

5. Conclusions

BIA Fat mass appears to be hindered by abnormal hydration distribution when adipose tissue plays the ECW expansion role. Probably inclusion of PhA might mitigate such hurdle.

Supplementary Materials: The following supporting information can be downloaded at: www.mdpi.com/xxx/s1, Figure S1: title; Table S1: title; Video S1: title.

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Data Availability Statement: The data supporting this study's findings are available from the corresponding author upon reasonable request.

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